

Phase control and measurement in digital microscopy

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Summary

The ongoing merger of the digital and optical components of the modern microscope is creating opportunities for new measurement techniques, along with new challenges for optical modelling. This thesis investigates several such opportunities and challenges which are particularly relevant to biomedical imaging. Fourier optics is used throughout the thesis as the underlying conceptual model, with a particular emphasis on three-dimensional Fourier optics.

A new challenge for optical modelling provided by digital microscopy is the relaxation of traditional symmetry constraints on optical design. An extension of optical transfer function theory to deal with arbitrary lens pupil functions is presented in this thesis. This is used to chart the 3D vectorial structure of the spatial frequency spectrum of the intensity in the focal region of a high aperture lens when illuminated by linearly polarised beam.

Wavefront coding has been used successfully in paraxial imaging systems to extend the depth of field. This is achieved by controlling the pupil phase with a cubic phase mask, and thereby balancing optical behaviour with digital processing.

In this thesis I present a high aperture vectorial model for focusing with a cubic phase mask, and compare it with results calculated using the paraxial approximation. The effect of a refractive index change is also explored. High aperture measurements of the point spread function are reported, along with experimental confirmation of high aperture extended depth of field imaging of a biological specimen.

Differential interference contrast is a popular method for imaging phase changes in otherwise transparent biological specimens. In this thesis I report on a new isotropic algorithm for retrieving the phase from differential interference contrast images of the phase gradient, using phase shifting, two directions of shear, and non-iterative Fourier phase integration incorporating a modified spiral phase transform. This method does not assume that the specimen has a constant amplitude. A simulation is presented which demonstrates good agreement between the retrieved phase and the phase of the simulated object, with excellent immunity to imaging noise.

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Declaration of originality

In this thesis I have acknowledged the contributions to my research made by my colleagues and collaborators. I have also cited the literature as appropriate. All other work presented is mine alone.

Significant contributions and collaborations included the following:

- Chapter 3: It was Colin Sheppard's suggestion to extend the transfer function theory from his papers (Sheppard et al., 1994; Sheppard and Larkin, 1997) in order to deal with arbitrary pupil functions. Andreas Schönle gently pointed out a mathematical error in the article which chapter 3 is based on (Arnison and Sheppard, 2002), enabling me to correct the error while preparing this thesis.
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Publications and presentations

Chapters 3–5 and chapter 7 are based on the work presented in the following publications:

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- Arnison, M. R., Cogswell, C. J., Sheppard, C. J. R., and Török, P. (2003) “Wavefront coding fluorescence microscopy using high aperture lenses,” in P. Török and F.-J. Kao (Eds.), *Optical imaging and microscopy: techniques and advanced systems*, vol. 87 of the Springer series in optical sciences, chap. 6, pp. 143–165, Springer-Verlag, Berlin.
- Arnison, M. R., Larkin, K. G., Sheppard, C. J. R., Smith, N. I., and Cogswell, C. J. (2004) “Linear phase imaging using differential interference contrast microscopy,” *J. Microsc.*, **214**(1), 7–12.

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- C. J. Cogswell,* M. R. Arnison, E. R. Dowski Jr., S. C. Tucker, and W. T. Cathey, “Extended–depth–of–focus fluorescence microscope made possible using wavefront coding,” *Focus on Microscopy*, (Shirahama, Japan, 2000).
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- W. T. Cathey,* M. R. Arnison, C. J. Cogswell, and E. R. Dowski Jr., “Large depth of field in fluorescence imaging of live cells,” *Optical Society of America Annual Meeting*, (Rhode Island, USA, 2000).
- C. J. Cogswell, M. R. Arnison,* E. R. Dowski Jr., S. C. Tucker, and W. T. Cathey, “Wavefront coding gives rise to a fast extended–depth–of–focus fluorescence microscope,” *Optics Within the Life Sciences VI*, (Sydney, Australia, 2000).
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Acronyms, abbreviations and conventions

\Leftrightarrow	Fourier transform relation
\otimes	convolution
\star	correlation
1D, 2D, 3D	one dimension, two dimensions, three dimensions
α	aperture half-angle
axial	parallel to the optical axis, z
amplitude	amplitude a of a complex field $ae^{i\phi}$
CCD	charge-coupled device
CPM	cubic phase mask
DC	direct current, i.e. image background or bias
DIC	differential interference contrast
EDF	extended depth of field
FITC	fluorescein isothiocyanate, a fluorescent dye
$f(x, y, z)$	functions in real space are usually lower case
$F(m, n, s)$	equivalent functions in Fourier space are often upper case
g'	projection of function g
$\mathcal{F}\{h\}$	Fourier transform of function h
f	vectors are set in boldface
FFT	fast Fourier transform
$k_0 = 2\pi/\lambda_0$	vacuum wave number for light of wavelength λ_0
lateral	orthogonal to the optical axis
$\mathbf{m} = (m, n, s)$	vector in Fourier space, unit directional vector

n	refractive index
NA	numerical aperture
OTF	optical transfer function
paraxial	approximate scalar field propagation for small angles to the optical axis
phase	phase ϕ of a complex field $ae^{i\phi}$; optical path length variations
PSF	point spread function
SNR	signal to noise ratio
transverse	orthogonal to the optical axis
vectorial	high aperture electromagnetic focusing theory
wave	unit of phase (2π radians)
widefield	conventional microscope imaging, without pupil filters
$\mathbf{x} = (x, y, z)$	vector in real space

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