

2.5. The Effect of Fluoride on Osteocalcin Levels

Dandona *et al.* (1988) administered NaF to healthy male subjects for three weeks to test whether the administration of NaF *in vivo* had an effect on osteocalcin concentration. The mean osteocalcin at three weeks was significantly higher than the pre-treatment mean. Six weeks after the cessation of fluoride treatment, the mean serum osteocalcin concentration had returned to the pre-treatment baseline. They concluded that fluoride in normal subjects over a short period increases serum osteocalcin and probably stimulates osteoblastic activity.

Srivastava *et al.* (1989) analyzed sera from patients with skeletal fluorosis and showed for the first time that patients with fluorosis have markedly elevated osteocalcin. This was evident even in the presence of subnormal concentrations of clinical vitamin D and calcium. This is relevant because it has previously been shown that 1,25(OH)₂D (the activated form of vitamin D) stimulates osteocalcin production by *in vitro* osteoblast cultures, that clinical vitamin D deficiency may prevent an increase in osteocalcin concentrations in response to parathyroid hypersecretion, and that the administration of 1,25(OH)₂D stimulates osteocalcin *in vivo* (Zerwekh *et al.*, 1985). The stimulatory effect of fluoride on osteocalcin production in patients with skeletal fluorosis would, therefore, appear to be greater than the inhibitory effect of vitamin D deficiency.

In a study investigating the value of slow release sodium fluoride treatment in the management of human osteoporosis, Pak *et al.* (1989) found that sodium fluoride therapy increases serum osteocalcin concentrations in osteoporotic patients and that serum osteocalcin concentrations correlated positively with the duration of treatment.

The evolution of bone changes induced by fluoride after the end of exposure was investigated in lambs by Chavassieux *et al.*, (1991). Along with an increase in bone formation it was found that serum osteocalcin was twice as high in treated animals compared with controls. In a separate study, the same investigators used a different sample group of ewes in which the early effects of two doses of sodium fluoride on bone remodelling were investigated.

One group of ewes received 1mg NaF/kg/day whilst the other group received a five-fold greater dose. Bone fluoride content significantly increased in the latter group along with osteoid perimeter and serum osteocalcin values (Chavassieux *et al.*, 1991). In a later study investigating the effects of sodium fluoride on human osteoblastic cultures, however, Chavassieux *et al.* (1993) found that the short term increase in osteocalcin expression by these cells is reversed upon longer exposure of the culture to this anabolic agent over four months.

The effect of mitogenic doses of sodium fluoride on osteocalcin in the rat model was investigated by Ohta *et al.*, (1995), who found that serum osteocalcin levels were significantly increased together with mineral apposition rate and bone formation rate in fluoride-treated rats as opposed to controls.

2.6. Osteocalcin and Tooth Movement

While the study of bone biology using cultured cells has proved useful, inherent artefacts in the *in vitro* system limit extrapolation to the *in vivo* system. This is due to the difficulty in recapitulating the sequence of differentiation events in intact bone during exposure to environmental osteogenic stimuli, such as hormones, growth factors or mechanical stress. Hence, the animal model of orthodontically-facilitated tooth movement has provided a means by which the dynamics of bone remodelling can be more accurately investigated.

The orthodontic movement of murine teeth was used by Pavlin and Gluhak-Heinrich (2001) to elucidate the response of osteocalcin to mechanical stimuli over a period of 14 days. After 24 hours of applied force, there was an inhibition of osteocalcin expression by 80%, followed by a marked four-fold induction at day two. Osteocalcin expression peaked six-fold at day four, then fell. However, the levels remained over four-fold higher compared with controls at day six. These results suggested a relatively early expression of osteocalcin in differentiating osteoblasts.

Hence, this mouse osseoinductive model was found to provide direct *in vivo* evidence that the osteocalcin gene is mechanically induced in osteoblasts much earlier than the mineralization stage, since its high expression can be followed from the early stages of matrix deposition (two days post-stimulation), on the surface of the newly deposited osteoid, as well as in the cells deeply embedded in and surrounded by osteoid.

Interestingly, the distribution of high osteocalcin-expressing cells across the thickness of new osteoid indicates higher levels of synthesis on the surface and in the middle portion of the osteoid than at the osteoid/bone junction. This refutes the idea of exclusive osteocalcin expression in mature osteoblasts, *i.e.* in a late stage of differentiation.

In the light of the results from osteocalcin-deficient mice and a proposed suppressive role of osteocalcin in bone formation (Ducy *et al.*, 1996), its up-regulation in the areas of active deposition of bone matrix in the mouse orthodontic model is consistent with its possible role as a determinant of the rate of mechanically induced bone remodelling. Furthermore, Pavlin *et al.*, (2001) showed that the temporal progression of the mechanically-induced osteoblast phenotype in the murine model occurs very rapidly. This suggests that physiologically relevant mechanical osteoinductive signals *in vivo* are targeting a population of committed osteoblast precursor cells that are capable of rapidly responding by entering a differentiation pathway and initiating an anabolic skeletal adaptation process.

There are also significant differences in the genetic responses of cementoblasts and osteoblasts to mechanical stimulation.

Pavlin *et al.* (2001) found that there was only a moderate stimulatory treatment effect on the expression of osteocalcin expression in cementoblasts (similar induction of osteocalcin expression in both cementoblasts of acellular cementum and cementoblasts of cellular cementum), compared to a six-fold induction in osteoblasts.

Local administration of 1, 25-dihydroxyvitamin D₃, or prostaglandin E₁ has been shown to accelerate experimental tooth movement (Collins and Sinclair, 1988; Yamasaki *et al.*, 1980). Both chemicals act as potent inducers of bone resorption *in vitro* and *in vivo*. Repeated injections of prostaglandin E₁ in rat alveolar bone produce marked changes in bone morphology with increased resorption at the site where the drug was infiltrated. Administration of 1, 25-dihydroxyvitamin D₃ has been reported to induce an increase in enlarged osteoclasts on the bone surface.

In contrast, local osteocalcin administration in the rat model has no appreciable effect on the bone surface (Kobayashi *et al.*, 1996). Osteocalcin was found to induce mature osteoclasts on the pressure side of orthodontic tooth movement, not on the tension side. This suggested that osteocalcin has an additive effect on the rate of orthodontic tooth movement through the enhancement of orthodontic tooth movement on the pressure side.

In a similar experiment involving the local injection of osteocalcin adjacent to rat molars over a longer period of time, Hashimoto *et al.* (2001) came to the same conclusion.

They suggested that osteocalcin might act as a chemoattractant for osteoclast precursor cells and an enhancer of maturation of multinuclear osteoclasts on the pressure side, where it may act in concert with bone resorbing factors (such as macrophage colony-stimulating factor [M-CSF]).

This then gives rise to an appropriate microenvironment for osteoclastogenesis. It was shown that there was acceleration of tooth movement following local application of osteocalcin in the early experimental period. Histological examination revealed that this acceleration was due to enhanced recruitment of osteoclasts. In contrast to the early days of the experiment, osteocalcin did not show an additive effect on the rate of orthodontic tooth movement towards the end of the ten day experimental period.

Previously, it has been shown that the chemotactic activity of osteocalcin for human peripheral monocytes (osteoclast precursor cells) displayed a bell-shaped dose-response curve. In addition, the serum osteocalcin level increased in the later phase of tooth movement in rats (King and Keeling, 1995). It is therefore possible that the increase in serum osteocalcin associated with tooth movement may diminish the effect of exogenous osteocalcin in the later period of tooth movement (Hashimoto *et al.*, 2001).

King and Keeling (1995) examined alveolar bone turnover and orthodontic tooth movement following appliance decay using closed coil springs in the rat model.

They observed that 93% of appliance activity was lost at day 16, at which time a second wave of bone remodelling began, with abrupt inhibition of ongoing bone formation and the initiation of a second wave of bone resorption. This was accompanied by a parallel rise in the amount of serum osteocalcin detected. The spike in osteocalcin values reached a nadir at day 22 when experimentation was concluded. They interpreted this data as being predictive of a second wave of bone formation (which did not eventuate due to premature conclusion of the experiment) rather than being representative of the occurring resorption.

2.7. Orthodontic Force Systems

2.7.1 Duration of Force

Frequency and duration of force application are known to be significant characteristics of the mechanical stress stimulating bone remodelling. Reitan (1951) reported on movement of dog incisors when application of force was discontinued for 20 seconds every ten minutes or for two minutes every two hours over 36 hours and stated that the amount of tooth movement was the same with continuous force. Gibson *et al.* (1992) reported that only one hour of force application was effective for mesial movement of rat molars.

In contrast, Konoo (1988) reported that force application of one hour per day for 14 days was not effective in moving molars in rats. Davidovitch and Shanfeld (1975) demonstrated that at least four hours of continuous force was required to increase the level of cyclic nucleoside that stimulated cell specialization.

Proffit (1999) insisted that there was a threshold of duration of force application for initiating clinical tooth movement. He also suggested that a loading time of more than six hours was effective for tooth movement and that a 24-hour, continuous force was optimal.

In all of these aforementioned studies, various force magnitudes, durations, and methods were used but the precise relationship between force duration and tooth movement remain unresolved. On the other hand, with substantially different forces, rates of tooth movement may be almost the same among or within individuals (Steiner *et al.*, 1981).

These individual differences in tooth movement characteristics are possibly related to individual variation in the structure of and cellular activity within the periodontal ligament and alveolar bone (Steigman and Michaeli, 1981) or to localized differences in the expression of factors such as cytokines and growth factors (Bridges *et al.*, 1981).

Interrupted orthodontic forces have also been shown to produce tooth movement similar to that generated by continuous forces with less damage to the structures of the periodontal ligament (Gibson *et al.*, 1992). In a series of experiments, King and his associates tested the relationship between force magnitude, duration, and frequency. Several conclusions emerged that supported previous research findings.

Light short-term or cyclic force applications can alter tooth position in a way comparable to light continuous forces. Significant amounts of bone turnover and remodelling events consistent with the direction of loading, and associated with tooth movement, continue for an indeterminate period after appliance decay, or appliance removal (King *et al.*, 1995).

An interesting finding in a diurnal orthodontic rat study by Igarashi *et al.* (1998) was that there was no significant difference in tooth movement between the light-period group and the whole-day group. This infers that the intermittent application of force for 12 hours (07:00 to 19:00) can produce tooth movement comparable to that produced by continuous force in rats. Previous studies both in animals (Gibson *et al.*, 1992) and human beings (Stutzmann and Petrovic, 1984) have shown that the application of intermittent or short-term forces for less than 24 hours are as effective as, or even more effective than continuous orthodontic force. However, it is possible that this might only be true when the force is applied at certain times of the day (during resting periods).

2.7.2 Generation of a Constant Orthodontic Force

Efficient, biological tooth movement by means of light continuous forces is the preferred treatment modality in contemporary orthodontics. In the application of orthodontic force, consideration of the maximum force of the appliance and the load-deflection rate of the deactivation curve are of paramount importance.

2.7.2.1 Superelastic Coil Springs

To this end, Von Fraunhofer *et al.* (1993) compared the force delivery by NiTi coil springs to that provided by comparable stainless steel springs and found that the former delivered optimal forces for orthodontic tooth movement over a longer activation range than the latter. Superelastic springs also offer superiority to other materials in that they are resistant to permanent deformation. Superelastic coil springs are able to deliver a constant force over a long range by virtue of the crystalline transition between austenite to martensite. This property in combination with the associated low stiffness and large springback is desirable in the choice of a model for orthodontic movement (Melsen *et al.*, 1994).

Two previous clinical studies investigated the efficiency and consistency of space closure with elastic modules compared to 100g, 150g and 200g Sentalloy nickel-titanium closed coil springs (Samuels *et al.*, 1993; Samuels *et al.*, 1998).

These studies both concluded that these springs produced more consistent space closure than elastic modules. A more recent randomized clinical trial conducted by Dixon *et al.* (2002) confirmed this finding, showing that superelastic NiTi springs had the advantage of giving significantly quicker and more consistent rates of space closure than elastic chain or active modules.

In a study of force systems developed from coil springs supplied by different manufacturers, Melsen *et al.* (1994) found that only the Sentalloy coil springs from GAC exhibited the behaviour of superelastic wire. In a study of the force characteristics of these same GAC superelastic closed coil springs, Tripolt *et al.* (1999) determined that the light springs (100g) delivered a more constant force during unloading than the medium (150g) and heavy springs (200g).

3. References

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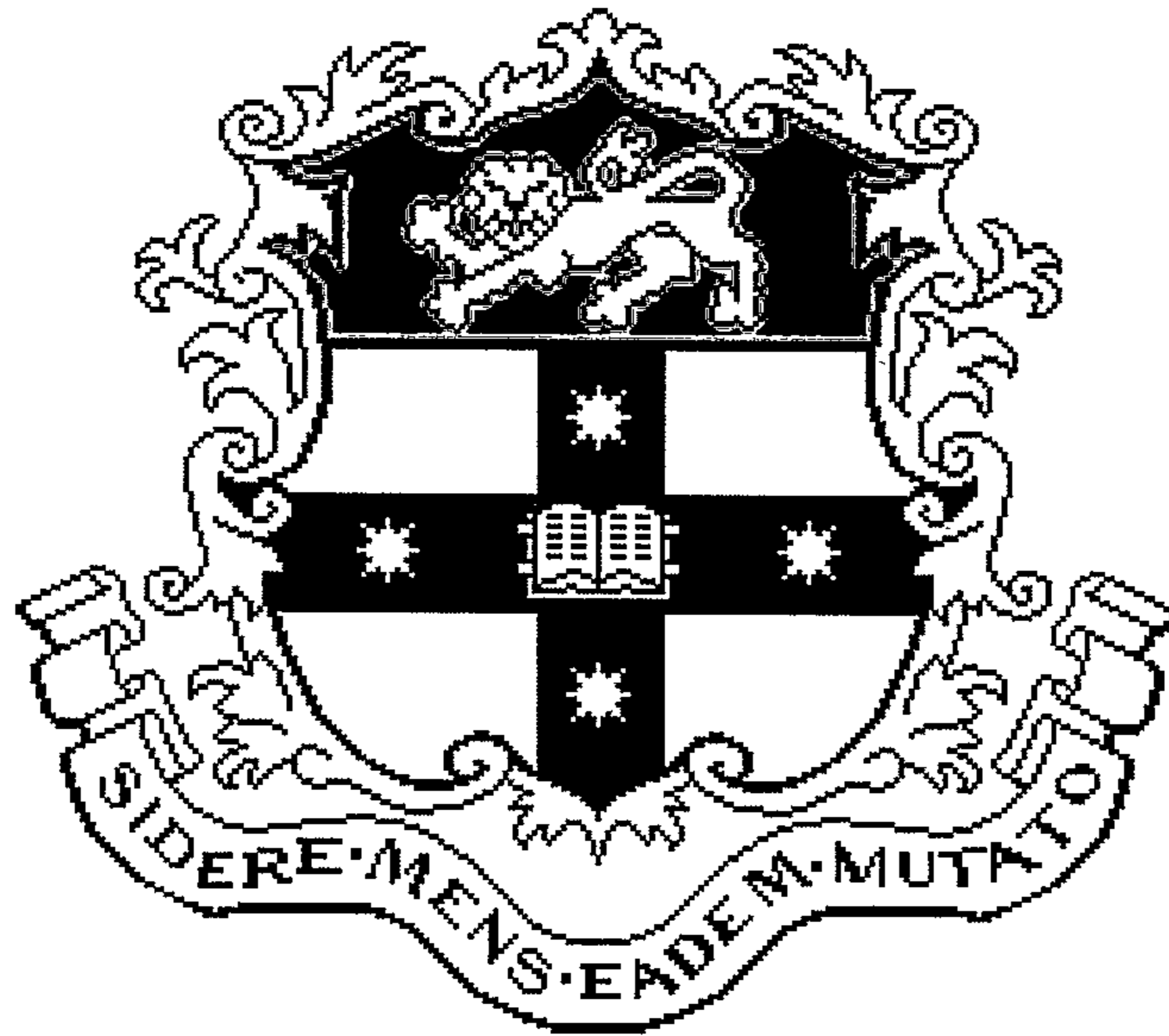
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4. Manuscript



**The effect of fluoride administration on rat
serum osteocalcin expression during
orthodontic tooth movement**

Abstract

Osteocalcin is a bone-protein that has previously been used as a marker of bone turnover. The precise role of this protein in bone remodelling has as yet not been fully elucidated, however, it has been shown to be instrumental in the activation of osteoclastic bone resorption via its effect on osteoblasts. Fluoride influences bone growth by acting as a mitogenic agent for osteoblasts. This study utilises a rodent model to determine the effects of fluoride administration on systemic osteocalcin during orthodontic tooth movement. Thirty-two, eight week old, female Wistar rats were divided into four groups for this experiment. The first experimental group of rats (n=10) were fed a normal laboratory diet and distilled water (MilliQ). The second experimental group of rats (n=10) had the same diet with the addition of fluoridated water. The third (n=6) and fourth (n=6) groups were used as control groups. These did not undergo orthodontic tooth movement and were given fluoridated (100ppm NaF) and non-fluoridated water *ad libitum*. Both fluoridated and non-fluoridated experimental samples had 100g NiTi coil springs secured to the lower incisor and left first molar tooth to instigate orthodontic tooth movement for a period of 14 days.

Phlebotomy was performed via the lateral tail vein prior to application of the orthodontic appliance and final blood samples were obtained via cardiac puncture following sacrifice two weeks later. Serum was isolated from the samples following centrifuging at each stage of phlebotomy and an enzyme-linked immunosorbent assay (ELISA) was subsequently performed to determine osteocalcin levels in the various sample groups.

Orthodontic tooth movement using high, continuous forces was found to have a positive, statistically significant correlation with serum osteocalcin expression in the rodent model. The use of fluoride as a variable was found to increase the mean osteocalcin concentration, however, this was not statistically significant.

Keywords: Osteocalcin, fluoride, cementum, tooth movement, ELISA.

Introduction

Osteocalcin is a non-collagenous bone-, dentine-, and cementum-specific protein that comprises about 2% of the total protein in bone¹. Osteocalcin is a calcium-binding peptide synthesized almost exclusively by osteoblasts and odontoblasts².

The distribution of osteocalcin in the mammalian body is limited to the calcified tissues such as bone, tooth cementum, and dentine³. It is distinguished by its small size (5800 daltons) and the presence of gamma-carboxy-glutamic acid (Gla). In the presence of ionic calcium, the Gla residues allow a specific conformational change in the protein, which in turn promotes osteocalcin binding to bone mineral and subsequent accumulation in bone matrix. Osteocalcin binds weakly to free calcium ions and more tightly to calcium in hydroxyapatite crystals. Spectroscopic studies suggest that the molecule undergoes a conformational shift when associated with hydroxyapatite, partly as a result of electrostatic attraction between specific anionic residues in the protein and the calcium ions embedded in the face of the crystal⁴. These unique structural features of osteocalcin that dictate the association with calcium ions and Ca²⁺ mineral surfaces may confer on this protein the ability to modulate the mineral dynamics of alveolar bone and cementum.

The proposition that osteocalcin may function as a negative regulator for mineral apposition is supported by the observation that purified osteocalcin inhibits the spontaneous conversion of brushite to hydroxyapatite and inhibits the formation of hydroxyapatite crystals in supersaturated calcium/phosphate solutions *in vitro*^{5,6}.

Through this high affinity for calcium ions and hydroxyapatite, osteocalcin was thought to be important in the regulation of mineral apposition in calcified tissues⁷.

However, warfarin treatment to prevent gamma-carboxylation and hence accumulation of osteocalcin in mineralized matrix failed to demonstrate a defect in mineralization^{3,8}.

Glowacki *et al.*, (1991) used subcutaneous apatite in the rat model with and without osteocalcin treatment to demonstrate that osteocalcin might function as a matrix signal in the recruitment and differentiation of bone-resorbing cells⁹. The precise role of this protein in bone remodelling has as yet not been fully elucidated; however, it has been shown to be instrumental in the activation of osteoclastic bone resorption via its effect on both osteoblasts and osteoclasts.

Liggett *et al.* (1994) provided support for this hypothesis with the observation that osteocalcin promotes differentiation of osteoclast progenitor cells from murine long-term bone marrow cultures in the presence of colony-stimulating factor (M-CSF) and granulocyte-macrophage stimulation factor (GM-CSF), but not in the absence of these factors. M-CSF has been shown to be a crucial factor in osteoclastogenesis¹⁰.

In vitro experiments have proved that osteocalcin is chemotactic for monocytes and osteoclasts in addition to activation of initial adherence of pre-osteoclasts in a dose-dependent manner¹¹.

Ducy *et al.* (1996) generated osteocalcin-deficient mice using embryonic stem cell technology and subsequent histomorphometry indicated that the lack of osteocalcin led to an increase in bone formation and an increase in osteoclast number in the bones of the osteocalcin-deficient mice¹².

To the same end, Wolf (1996) used mice that lacked the genes for osteocalcin to study the function of the bone protein¹³. These osteocalcin-deficient mutants developed increased bone density and thickness. Their osteoblasts deposited more bone matrix than those of the wild-type mice. This too, infers that osteocalcin is a negative regulator of bone formation.

Serum osteocalcin reflects the 10-40% of osteocalcin produced that is not incorporated into the bone matrix. The majority of osteocalcin secreted by the osteoblast is deposited in extracellular bone matrix and serum osteocalcin represents the fraction of total osteocalcin that has not adsorbed to hydroxyapatite in the mineralized tissues. Comparable levels of osteocalcin are found in both serum and plasma samples of humans and animals⁵.

The normal degree of coupling between bone formation and resorption is disturbed in orthodontic tooth movement¹⁴. This occurs at an early stage at sites of pressure and later in sites of tension.

These imbalances facilitate tooth relocation by removing bone ahead of the tooth and depositing it behind. In this respect, this quantitative uncoupling of bone remodelling is similar to the process of osteoporosis.

The anabolic action of fluoride is well established. The osteogenic property of increasing bone mass through stimulating bone formation is the basis for the previous use of fluoride as a therapeutic agent in osteoporosis¹⁵⁻¹⁸.

Fluoride influences bone growth by acting as a mitogenic agent for osteoblasts¹⁹ and may also act as an inhibitory stimulus to osteoclasts, although this is less well understood due to the possible side-effect of fluoride-induced secondary hyperparathyroidism²⁰. It has been shown that osteoblast precursors are more sensitive to fluoride than mature osteoblasts and that the *in vivo* effects of fluoride on bone formation may be mediated by stimulating proliferation and differentiation of committed osteoblast precursors in cancellous bone²¹.

Fluoride also alters the composition and crystalline state of mineral with the substitution of hydroxyl ions by fluoride ions. Fluoroapatite has a greater crystallinity, larger crystal size, and lower aqueous solubility than hydroxyapatite²². Moreover, a mixture of fluoroapatite and hydroxyapatite has been shown to be less soluble than either component individually²³. Hence, changes in apatite crystallinity could explain the inhibition of mineralised tissue resorption seen after fluoride treatment.

There is *in vitro* evidence that fluoride decreases the number of resorption lacunae as well as the amount of bone resorbed per osteoclast²⁴. Increased resistance to dissolution by osteoclastic enzymes as well as high levels of fluoride liberated from fluoride-containing bone during the resorptive process might inhibit osteoclastic activity and explain this effect of fluoride²⁵.

The aim of this study was to investigate the serum osteocalcin levels that could be elicited with constant orthodontic force levels from a superelastic coil spring applied to rat molar teeth using fluoride as a variable.

Null Hypotheses

1. That there is no discernible difference in the measurements of serum osteocalcin in rats subjected to a high fluoride diet compared to those rats limited to distilled water intake following the application of high orthodontic forces to mandibular molar teeth.
2. That there will be no increase in systemic osteocalcin following the application of high orthodontic forces to mandibular molar teeth in rats.

Materials and Methods

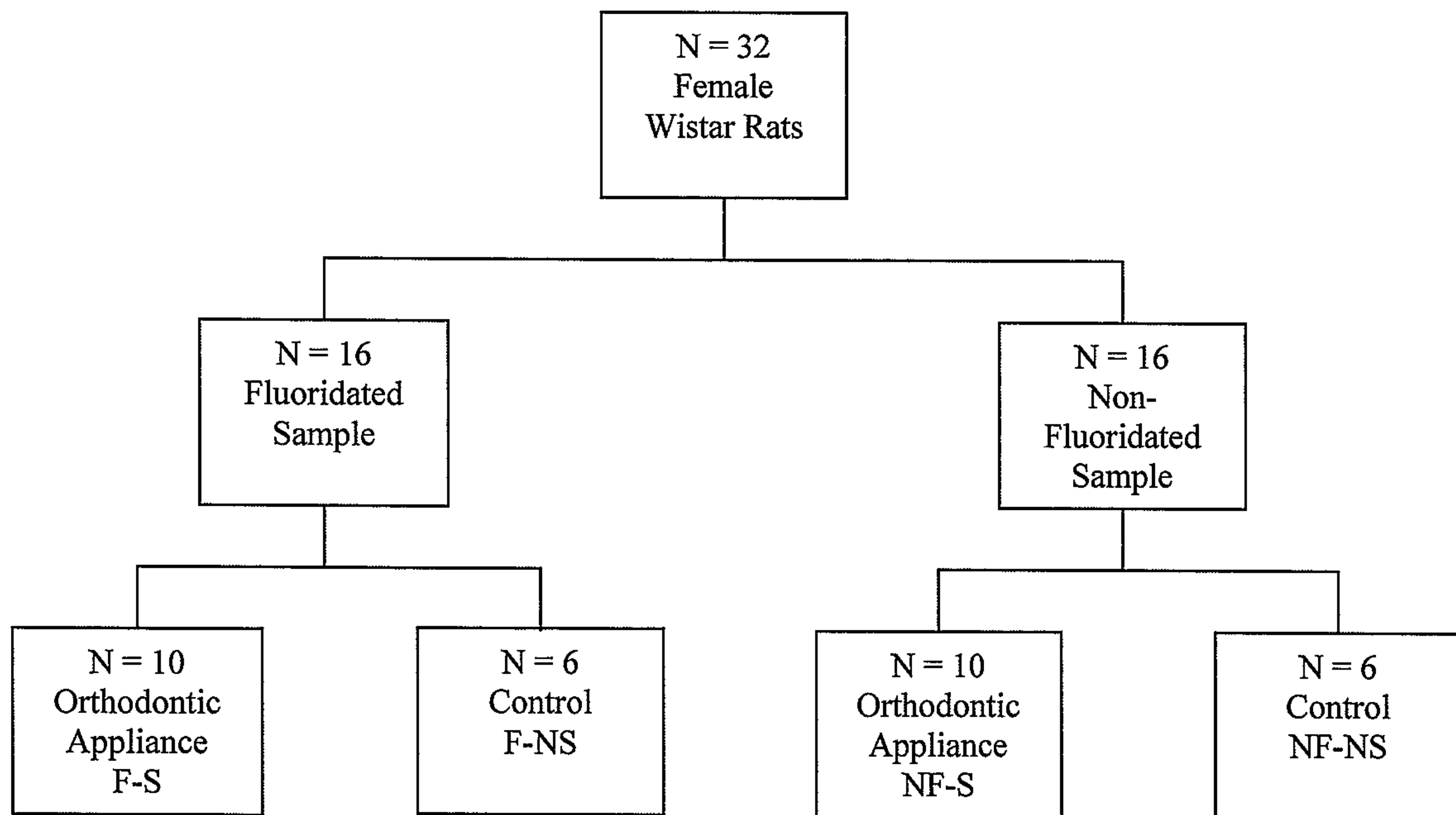
Animals

Thirty-two, 7-8 week old female, Wistar rats weighing approximately 210 g were obtained from the Westmead Animal Holding Facility and conditioned in experimental cages for at least 24 hours before use in experiments (Ethics approval: Westmead Hospital Animal Ethics Committee Project no. 134.12-03) (Figure 1).

The rats were divided into four groups for the purposes of this experiment. The first group of rats (n=10) were fed a standard pellet diet and distilled water (MilliQ) *ad libitum*. The second group of rats (n=10) consumed the same diet with the addition of fluoridated water (100ppm NaF) *ad libitum*. The third (n=6) and fourth (n=6) groups served as controls. These rats did not undergo orthodontic tooth movement and were given fluoridated and non-fluoridated water *ad libitum* respectively.

Figure 1

NF-NS = non-fluoridated control (no springs)
NF-S = non-fluoridated rats with springs
F- NS = fluoridated control (no springs)
F-S = fluoridated rats with springs



Appliance placement

A superelastic, fixed, closed coil spring appliance was used to facilitate the mesial movement of the mandibular lower left first molar (GAC International Inc., Central Islip, NY). The orthodontic force thus applied was approximately 100g (Figure 2). The duration of the experimental period was 14 days with no reactivation of the appliance during this time period.

The Nickel Titanium spring was ligated (with a stainless steel ligature) to the central incisor teeth and attached to the first lower left molar using a 3/0 black silk suture. The placement of appliances was performed under general anaesthesia, using Xylazine (10mg/kg) and Ketamine (10mg/kg).

Phlebotomy was performed via the lateral tail vein with a 26-gauge needle prior to application of the orthodontic appliance. Following clotting of the blood sample, centrifugation at 5000 rpm for five minutes was undertaken before serum transfer with further centrifugation at 10,000 rpm for five minutes. The supernatant serum was immediately isolated to avoid haemolysis, and then frozen at -70°C.

Following appliance application, the rodents were permitted to recover from anaesthesia before being placed into separate experimental cages. At the end of the experimental period of 14 days the rodents were euthanased with carbon dioxide asphyxiation before final blood collection via intracardiac sampling.

Sample Analysis

Osteocalcin Assay

An enzyme-linked immunoassay (ELISA) kit was used for the detection of osteocalcin (Biomedical Technologies Inc. Stoughton, MA 02072, USA).

Briefly, the capture antibody (mouse monoclonal anti-osteocalcin) was added to a microtitre plate and incubated overnight at 4°C. Following blocking and wash stages, standard solutions of osteocalcin and the test samples were added. Standard solutions were prepared by serial dilution of the re-hydrated standard osteocalcin provided by the kit manufacturer.

The standard curve obtained from these data was used to determine the concentration of osteocalcin detected in the eluted serum samples analysed in the assay.

Following a wash stage, the detection antibody, murine monoclonal antibody to osteocalcin conjugated to alkaline phosphatase, was applied to each well and incubated for 1hr at room temperature. After washing, 100µl of substrate solution, containing a chromogen was added to each well. The microtitre plate was incubated at room temperature for 24hrs. 100µl of stop solution (1N sulphuric acid) was then applied to each well. The plate was transferred to a plate reader and the absorbance of the colour reaction was measured at 450nm. Two separate ELISA kits were needed to assay all unknown samples in duplicate.

Results

Weight gain

The mean weight of the rats in the F-S, NF-S, F-NS and NF-NS groups were 225 ± 13 g, 228 ± 19 g, 219 ± 23 g and 221 ± 13 g respectively. All rats in the two groups that had orthodontic appliances placed under anaesthesia experienced some initial weight loss, which was not fully recovered during the experimental period. At the end of two weeks the non-fluoridated sample (NF-S) with appliances lost 16g and the fluoridated sample with appliances (F-S) lost 28g. Both control groups not receiving orthodontic appliances (F-NS, NF-NS) showed an increase in weight; 32g in the non-fluoridated sham and 21g in the fluoridated sham sample respectively.

Water consumption

Water consumption was monitored throughout the trial period and the average individual consumption of the rats receiving distilled water amounted to 16ml per day. The rats receiving fluoridated water (100 ppm NaF) consumed an average of 10ml per day.

Appliance activation

All closed coil springs retained greater than 200 per cent activation at the end of the experimental period, indicating that there was no significant deactivation of the appliances during this time.

Statistical analysis (Tables 1 and 2)

All statistical analysis was done with the assistance of SPSS (SPSS Chicago 60606, Illinois). Analysis of the raw data revealed there were three significantly aberrant values in the post-mortem samples (NF-S, F-S and NF- NS) which were two, three and four times the mean values for their sample groups respectively. Due to the large isolated deviations of these samples from the mean and their distance from the mean regression line, it seemed reasonable to exclude these values from statistical analysis in a second ANOVA.

The influence of inter-kit variation

Two separate ELISA kits were needed for this experiment and, therefore, the possibility of inter-kit variation interfering with the interpretation of subsequent results was a possibility. Statistical analysis using ANOVA, however, refuted this influence as an obfuscating factor with a p-value of 0.864 (significance was taken as $p < 0.05$).

The effect of springs on osteocalcin expression

The orthodontic movement of the rat molar elicited by the appliance resulted in a marked increase in mean osteocalcin levels, which only achieved a level of moderate statistical significance ($p < 0.051$) with the univariate analysis of variance. However, if the three aforementioned aberrant values are removed from the analysis, then this variable attains a moderate level of significance ($p < 0.03$).

The effect of fluoride on osteocalcin

Osteocalcin expression was found to remain close to baseline levels when control rats from the non-fluoridated group were compared with the fluoridated shams. ANOVA was used for statistical analysis of variables and there was found to be no statistically significant increase in osteocalcin in rats without orthodontic appliances, regardless of fluoride consumption ($p < 0.524$) (Figures 3 and 4).

The effect of fluoride and springs on osteocalcin expression

Although there was a mean increase in osteocalcin concentration associated with the F-S sample, fluoride together with the use of the orthodontic appliance was not found to have a statistically significant interaction with one another on osteocalcin expression overall (Figures 5 and 6).

Discussion

It has previously been shown that fluoride consumption in rats at levels in excess of 50mg/mL has an adverse effect on weight of the animals compared with controls²⁶, and although this was found to be the case in this study, it is not possible to determine a direct correlation. This weight loss may, however, also be explained by the lower water consumption of the fluoridated samples, due in part perhaps to the poor taste of the medium of fluoride administration.

Osteocalcin is markedly unstable *in vitro*^{27, 28}, rapidly degrading in samples at room temperature and at 4° C and is also sensitive to freeze-thaw cycles and haemolysis. Repeated freeze-thaw cycles have been shown to reduce immunoreactivity by up to 40%²⁹. Haemolysis decreases apparent osteocalcin concentrations, due to proteolysis by enzymes released from lysis of red blood cells³⁰. Given the inherent problems of sample stability and biological variability (including diurnal variation with circadian rhythm), there was an absolute need for continuity in the methodology for sample collection. This included the avoidance of haemolysis and freeze-thaw cycles as well as time-dependent phlebotomy during collection of the samples³¹.

Young rats were chosen because it has been shown that there is complete formation of dentine, cementum, alveolar bone and the periodontal ligament at eight weeks in this particular animal model³². In addition, young rats have been shown to recover rapidly from the surgical insult in orthodontic appliance placement³³.

Bridges *et al.* (1988) evaluated the effects of age on tooth movement and concomitant mineral density in the treated tissues of the rat³⁴. The absolute amount of tooth movement occurring in a cycle and the rate of tooth movement in the late part of the cycle were significantly greater in the younger animals (21-28 days old), while the total time required for a cycle was shorter in the younger animals. The "instantaneous" tooth movement was greater in the young animals than older animals (100 days old) and the control tissue mineral density was lower, suggesting that bone density may play a key role in this phase of the cycle. Mineral densities returned to control levels at

approximately the same rate in the tissues of both groups during the late part of the cycle, but the rate of tooth movement in the adult was less than in the younger animal.

This suggests that the proportions of bone formation to resorption are equivalent at comparable times in both groups, but that absolute amounts of each may be higher in the younger animals.

King and Fischlschweiger (1982) showed that when appliances were loaded with increasing amounts of force, the specific activity of bone resorption stimulators increased progressively³⁵.

This was highlighted by the study of Ashizawa and Sahar (1998) who moved rat molars mesially with a fixed coil-spring appliance using three different magnitudes of initial tensile force (27, 60 and 136g)³⁶. They found little or no relationship between the magnitude of the initial tensile force and the amount of new bone formation in the alveolar wall on the tension side during the initial stage of tooth movement. However, a heavy initial force (136g) produced a wide necrotic area of periodontal ligament, and delayed the bone remodelling that occurred on the pressure side. It was, therefore, decided to use a heavy force of 100g in this present study so that there would be a consistent and constant force during the experimental period, which would maximize the potential for indirectly observing hard tissue turnover. This in turn would increase the possibility of assessing the relationship between this hard tissue turnover and subsequent osteocalcin expression.

Studies that have utilized an antibody against the propeptide of osteocalcin have indicated that osteocytes are the primary source of osteocalcin in human bone, and that it may function by signalling osteoclasts and/or their precursors to initiate bone resorption⁸. Kagayama *et al.* (1997) investigated the expression of osteocalcin in Wistar rats³⁷. They found that all cells lining cellular cementum were positive for osteocalcin. They suggested that the osteocalcin expression of cementoblasts forming acellular cementum is similar to that of cells forming cellular cementum as well as osteoblasts and odontoblasts. Consistent with these observations, the cells engaged in the formation of cellular cementum (cementoblasts and cementocytes) were also found to be associated with large amounts of osteocalcin³⁸. Bronckers *et al.*, (1994) concluded that cementoblasts and cementocytes of cellular cementum produce osteocalcin and express an osteoblast-like, not an odontoblast-like phenotype³⁹. In addition, cells and matrices of surrounding alveolar bone were found to strongly express the bone protein.

Lu *et al.* (1999) applied orthodontic forces (50g) to mandibular rat molars, demonstrating higher distribution of osteoclastic cells on the alveolar bone than on the root surface, indicating that alveolar bone is more readily removed than the root surface⁴⁰. They also showed that cellular cementum may be resorbed more easily than acellular cementum due to its enhanced organic components and low mineralized structure. Hence, the dissolution of tooth structure as occurs during the process of physiologic tooth movement may result in the release of osteocalcin.

Local osteocalcin administration in the orthodontic rat model was found to induce mature osteoclasts on the pressured side of orthodontic tooth movement but not on the tension side⁴¹.

This suggests that osteocalcin has an additive effect on the rate of orthodontic tooth movement through the enhancement of orthodontic tooth movement on the pressured side. In a similar experiment involving the local injection of osteocalcin adjacent to rat molars over a longer period of time, Hashimoto *et al.* (2001) came to the same conclusion⁴².

They suggested that osteocalcin might act as a chemoattractant for osteoclast precursor cells and an enhancer of maturation of multinuclear osteoclasts on the pressure side, where it may act in concert with bone resorbing factors (such as macrophage colony-stimulating factor [M-CSF]). This then gives rise to an appropriate microenvironment for osteoclastogenesis. It was shown that there was acceleration of tooth movement following local application of osteocalcin in the early experimental period. Histological examination revealed that this acceleration was due to enhanced recruitment of osteoclasts. In contrast to the early days of the experiment, osteocalcin did not show an additive effect on the rate of orthodontic tooth movement towards the end of the ten-day experimental period.

Previously, it has been shown that the chemotactic activity of osteocalcin for human peripheral monocytes and osteoclast precursor cells displayed a bell-shaped dose-response curve. In addition, the serum osteocalcin level has been observed to increase in the later phase of tooth movement in rats⁴³. It is therefore possible that the increase in

serum osteocalcin associated with tooth movement may diminish the effect of exogenous osteocalcin in the later period of tooth movement⁴².

King and Keeling (1995) examined alveolar bone turnover and orthodontic tooth movement following appliance decay using closed coil springs in the rat model⁴³, unlike the present study, which used a continuous force. They observed that 93% of appliance activity was lost at day 16, at which time a second wave of bone remodelling began, with abrupt inhibition of ongoing bone formation and the initiation of a second wave of bone resorption. This was accompanied by a parallel rise in the amount of serum osteocalcin detected. The spike in osteocalcin values reached a nadir at day 22 when their experimentation period was concluded.

They interpreted these data as being predictive of a second wave of bone formation (which did not eventuate due to premature conclusion of the experiment) rather than being possibly being representative of the occurring resorption.

The orthodontic movement of murine teeth by Pavlin and Gluhak-Heinrich (2001) was used to elucidate the response of osteocalcin to mechanical stimuli over a period of 14 days⁴⁴. After 24 hours of applied force, there was an inhibition of osteocalcin expression by 80%, followed by a marked four-fold induction at day two. Osteocalcin expression peaked six-fold at day four, then fell. However, the levels remained over four-fold higher compared with controls at day six. These results suggested relatively early expression of osteocalcin in differentiating osteoblasts and much earlier than the mineralization stage.

In the light of the results from osteocalcin-deficient mice and a proposed suppressive role of osteocalcin in bone formation¹², its up-regulation in the areas of osteoblastic activity in the mouse orthodontic model is consistent with its possible role as a determinant of the rate of mechanically induced bone remodelling.

A role for osteoblastic involvement in the control of bone resorption was hypothesized by Rodan and Martin (1981)⁴⁵. The hypothesis suggested that resorbing agents, such as PTH and prostaglandins, induce a shape change in osteoblasts (via cAMP and Ca²⁺), which uncovers matrix for osteoclastic digestion, further enhancing subsequent resorption by releasing osteocalcin. This interdependent relationship of osteoblasts and osteoclasts in the orchestration of hard tissue remodeling may, therefore, be partly facilitated by osteocalcin.

There are also significant differences in the genetic responses of cementoblasts and osteoblasts to mechanical stimulation. Pavlin *et al.* (2001) found that there was only a moderate stimulatory treatment effect on the expression of osteocalcin expression in cementoblasts (similar induction of osteocalcin expression in both cementoblasts of acellular cementum and cementoblasts of cellular cementum), compared to a six-fold induction in osteoblasts⁴⁶.

Hence it was postulated that orthodontic tooth movement using heavy forces lead to the increased expression of serum osteocalcin from local sources including cementum and alveolar bone.

In this study, osteocalcin expression was indeed increased by the use of heavy orthodontic forces. The precise tissue of origin of the osteocalcin was, however, unable to be determined by the present methodology. The osteocalcin may have originated from local cementum degradation, alveolar bone dissolution or from local production by osteoblasts associated with the periodontal ligament and cementoblasts.

Singer *et al.* (1967) found that indirect resorption occurred in the absence of periodontal ligament hyalinization during tooth movement induced in fluoride-treated rats⁴⁷. There was found to be considerably less bone loss and osteoclastic activity in the fluoridated rats than in the non-fluoridated group, thus interfering with experimental tooth movement in the former. Much smaller forces in the form of elastomeric separating modules were used in this particular study than were used in the present study and this may explain the absence of hyalinization observed.

Cheng and Bader (1990) concluded that fluoride affects rat cortical and cancellous bone differently and that fluoride increases rat cancellous bone volume through trabecular thickening in a dose-dependent manner⁴⁸. This is most probably due to a combination of: reduced bone resorption, increased bone mineral packing density and increased size of individual bone mineral crystallite. This mirrors the findings in human subjects¹⁶.

The lack of intracortical (Haversian) remodelling in the rat may explain any difference in bone mass when compared with humans⁴⁹.

Fluoride incorporation into the skeleton is largely dependent upon remodelling (formative) surfaces, and very little response should be expected in cortical bone in rats. It has also been demonstrated that fluoride is generally more readily incorporated into cancellous bone than cortical bone⁵⁰ which may be seen to directly impact upon orthodontic tooth movement.

The evolution of bone changes induced by fluoride was investigated in lambs by Chavassieux *et al.* (1991)⁵¹. Together with an increase in bone formation it was found that serum osteocalcin was twice as high in treated animals as compared to controls.

The effect of mitogenic doses of sodium fluoride on osteocalcin in the rat model was investigated by Ohta *et al.*, (1995), who found that serum osteocalcin levels were significantly increased together with mineral apposition rate and bone formation rate in fluoride treated rats when compared to controls⁵². This was also seen in the present study, where mean increases in osteocalcin concentration were observed in the fluoridated, orthodontic appliance group. These increases were not, however, statistically significant and may have been a function of the small sample size.

If fluoride could indeed decrease the resorption of mineralized tissues then it might be expected that local expression of osteocalcin would reduce. If local osteocalcin

expression was expressed in a systemic concentration increase then this is not reflected in these aforementioned results.

Ingram *et al.* (1994) showed that the presence of an osteocalcin-rich matrix increased the recruitment and binding of osteoclasts and, therefore, osteocalcin was postulated to be a site-specific regulator of bone remodelling⁵³. As fluoride has been shown to be mitogenic to osteoblasts, then it is possible that the observed fluoride-induced increase in serum osteocalcin during this study may just be a biological representation of this anabolic process. Although there was no statistical significance with respect to osteocalcin expression in orthodontically-treated rodents exposed to fluoride, this may have been a function of the reduced power of the sample size and not necessarily, because of an absent interaction.

A further factor which may have affected the results is the lack of pre-treatment with fluoride. Concomitant exposure to fluoride during the period of experimentation may have reduced the potential for fluoride incorporation into the mineralized tissues and, therefore, reduced the manifestation of its protective mineralized tissue properties.

On the basis of these results Null Hypothesis No. 1 (that there is no increase in OC expression at a systemic level upon application of an orthodontic force in a rodent model) must be rejected. Null Hypothesis No. 2, (that the systemic intake of fluoride does not increase serum OC expression in a rodent model following orthodontic force application), however, cannot be rejected on the basis of the results obtained from this study.

Conclusions

The systemic expression of osteocalcin was found to be positively correlated with the local event of orthodontic tooth movement in this rodent model. Although the addition of fluoride as a variable was found to result in a mean increase in systemic osteocalcin expression, this increase was not found to be statistically significant.

The source of the increased osteocalcin observed as a result of the applied orthodontic forces was not able to be ascertained with the current methodology and therefore it was not possible to further clarify the nebulous role that this bone protein plays during the complex orchestration of mineralized tissue turnover. Further understanding of the biological implications of increased osteocalcin expression may therefore require further research into the *local* expression of this protein in the gingival crevice during orthodontic movement. Fluoride has previously been shown to have a protective role with respect to hard tissue demineralization and although this was not evident in the present study, pre-treatment of the experimental samples with fluoride may have provided more insight into the nature of this property with respect to osteocalcin expression.

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FIGURES

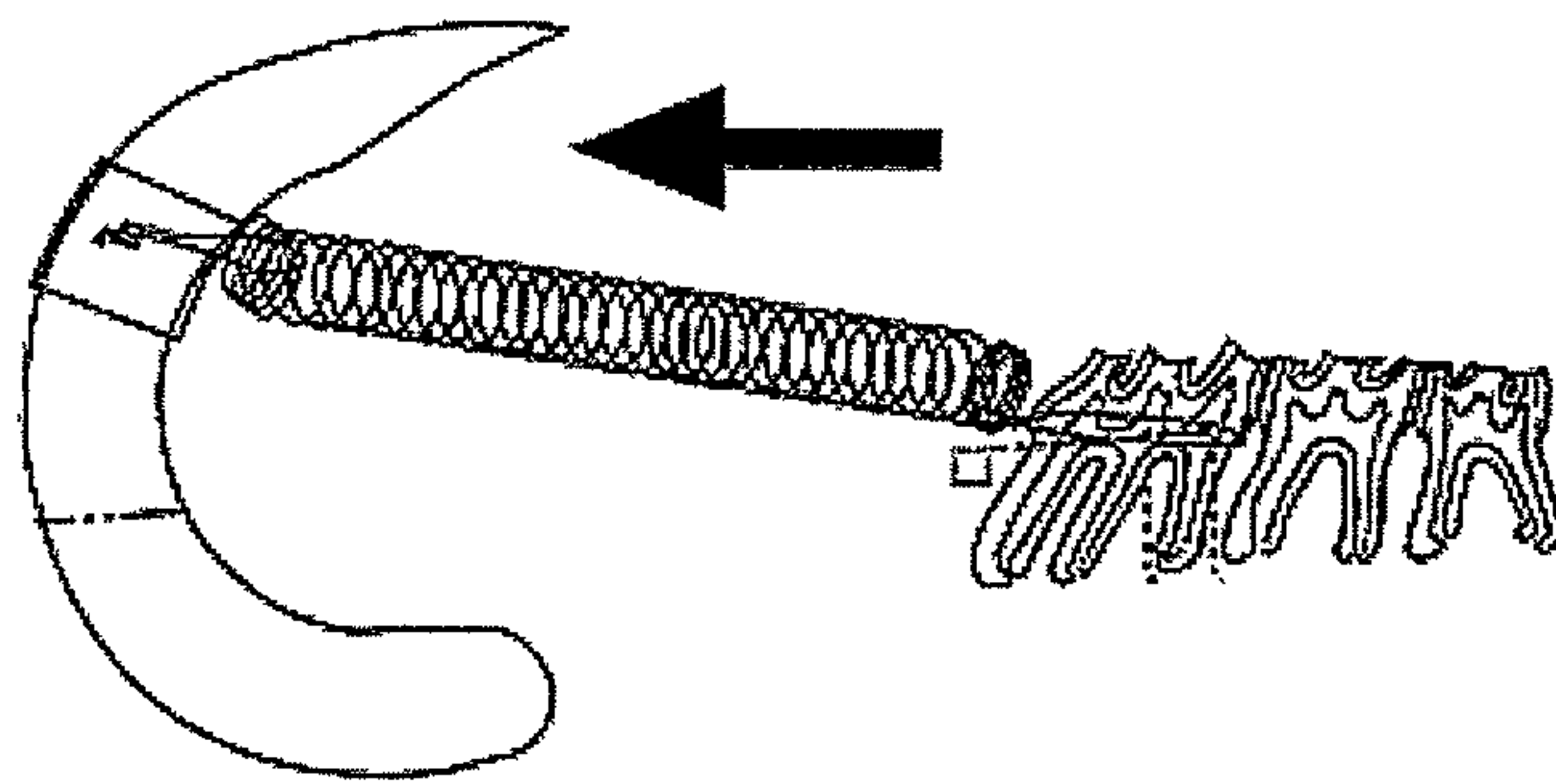


Figure 2. Diagrammatic representation of the orthodontic appliance applied to the mandibular incisors and rodent first molar teeth.

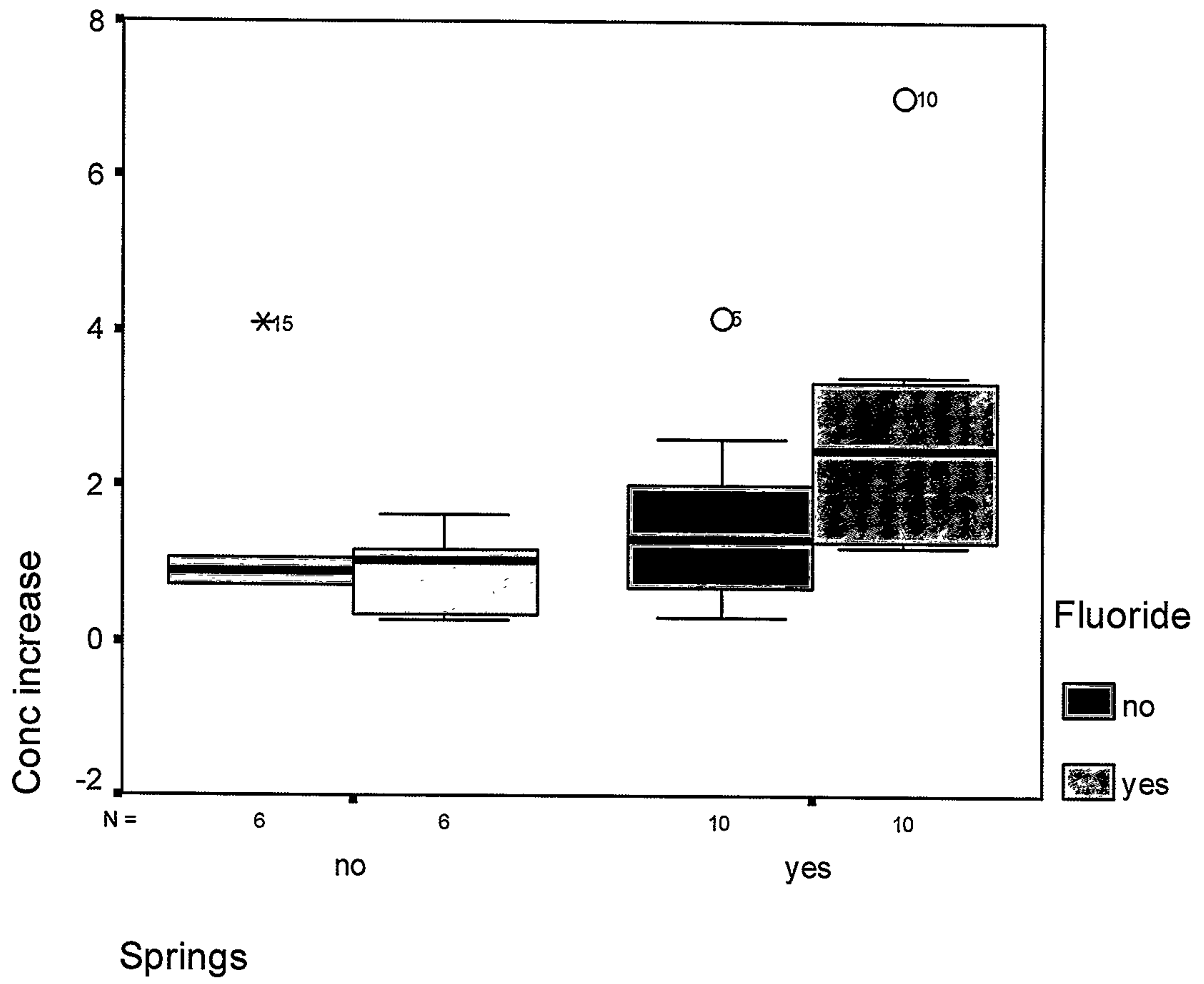


Figure 3. THE EFFECT OF FLUORIDE ON OSTEOCALCIN CONCENTRATION

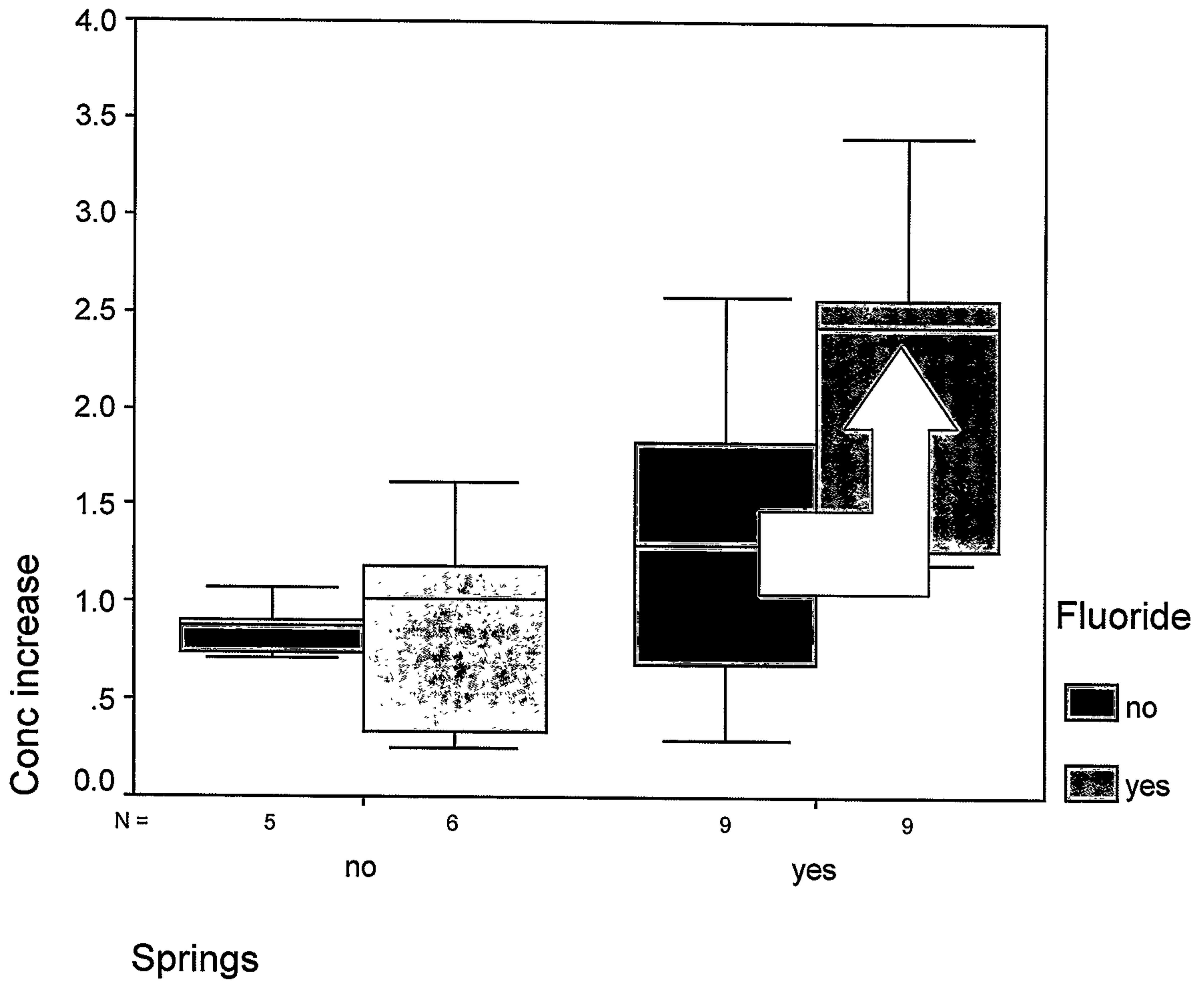


Figure 4. THE EFFECT OF FLUORIDE ON OSTEOCALCIN CONCENTRATION (FOLLOWING REMOVAL OF THREE ABERRANT VALUES).

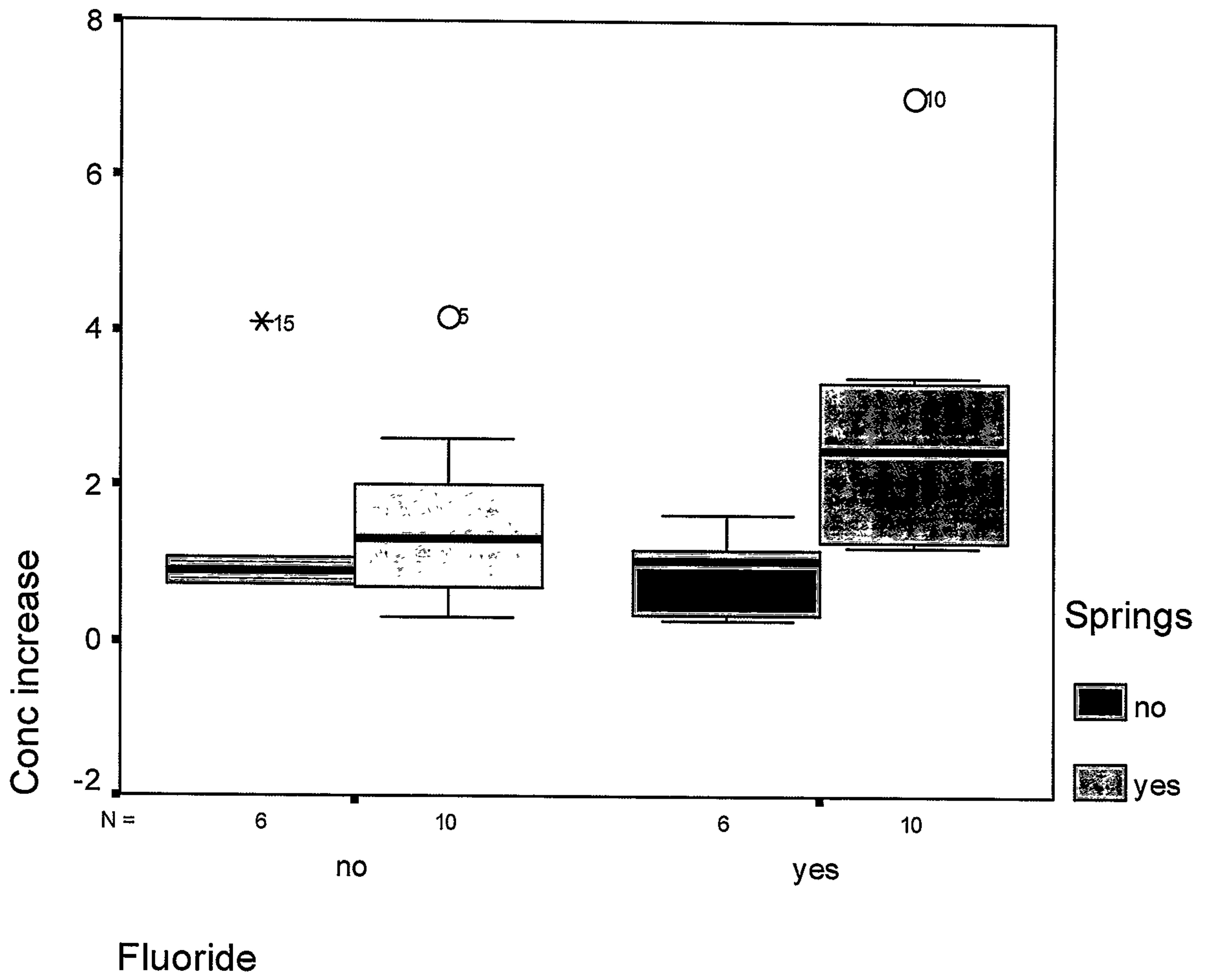


Figure 5. THE EFFECT OF SPRINGS ON OSTEOCALCIN CONCENTRATION

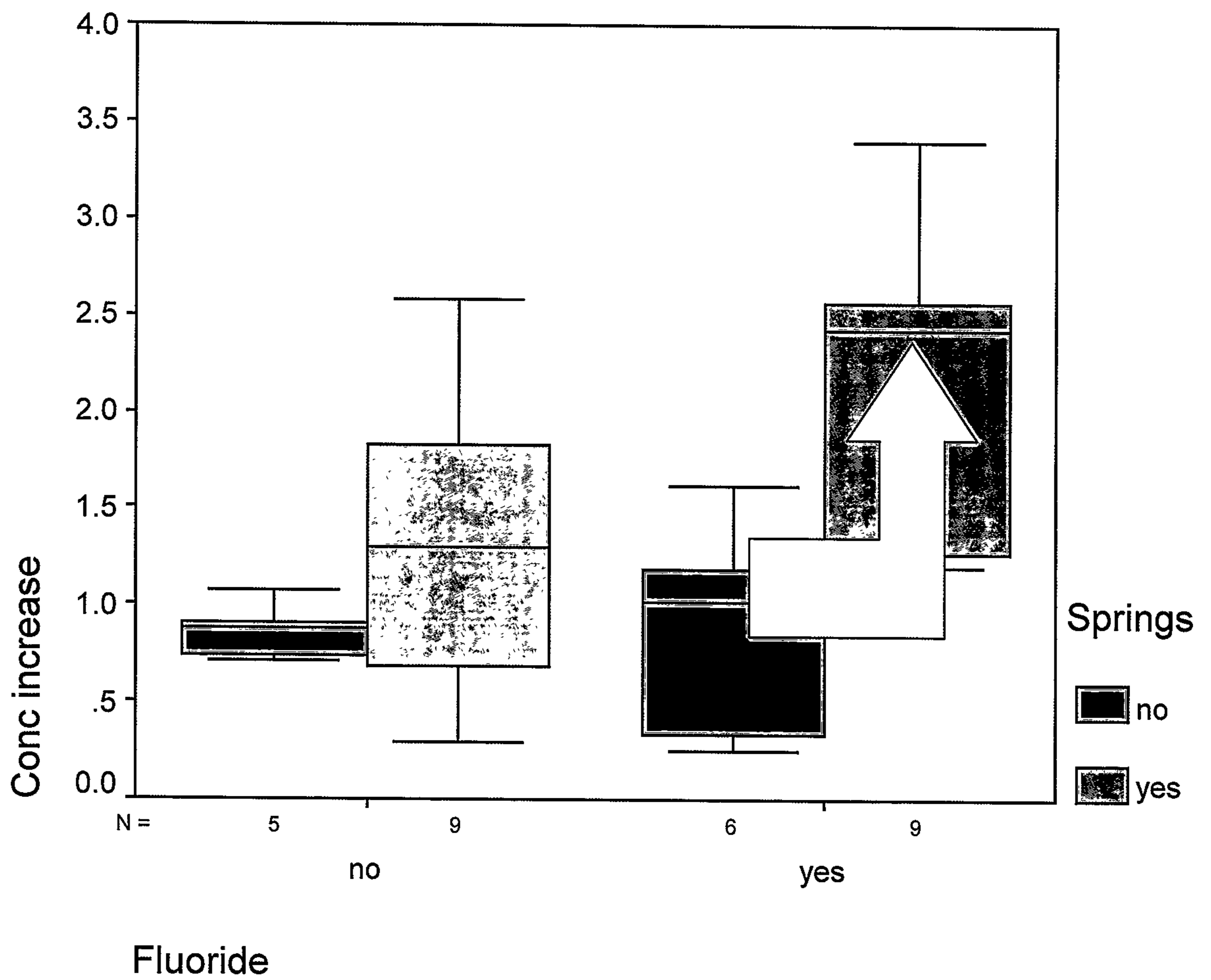


Figure 6. THE EFFECT OF SPRINGS ON OSTEOCALCIN CONCENTRATION (FOLLOWING REMOVAL OF THREE ABERRANT VALUES)

Table 1. Statistical Analysis of all Data

Tests of Between-Subjects Effects

Dependent Variable: DCC Conc increase

Source	Type III Sum of Squares	df	Mean Square	F	Sig.
Corrected Model	14.289 ^a	3	4.763	2.728	.063
Intercept	81.089	1	81.089	46.444	.000
FL	.727	1	.727	.416	.524
SP	7.276	1	7.276	4.167	.051
FL * SP	4.903	1	4.903	2.808	.105
Error	48.887	28	1.746		
Total	163.110	32			
Corrected Total	63.175	31			

a. R Squared = .226 (Adjusted R Squared = .143)

Table 2. Statistical Analysis with three aberrant values removed

Tests of Between-Subjects Effects

Dependent Variable: DCC Conc increase

Source	Type III Sum of Squares	df	Mean Square	F	Sig.
Corrected Model	9.013 ^a	3	3.004	6.347	.002
Intercept	47.119	1	47.119	99.534	.000
FL	1.595	1	1.595	3.369	.078
SP	5.132	1	5.132	10.840	.003
FL * SP	1.334	1	1.334	2.818	.106
Error	11.835	25	.473		
Total	79.531	29			
Corrected Total	20.848	28			

a. R Squared = .432 (Adjusted R Squared = .364)

Legend:

Fl- Fluoridated sample DCC- Osteocalcin

SP- Presence of springs

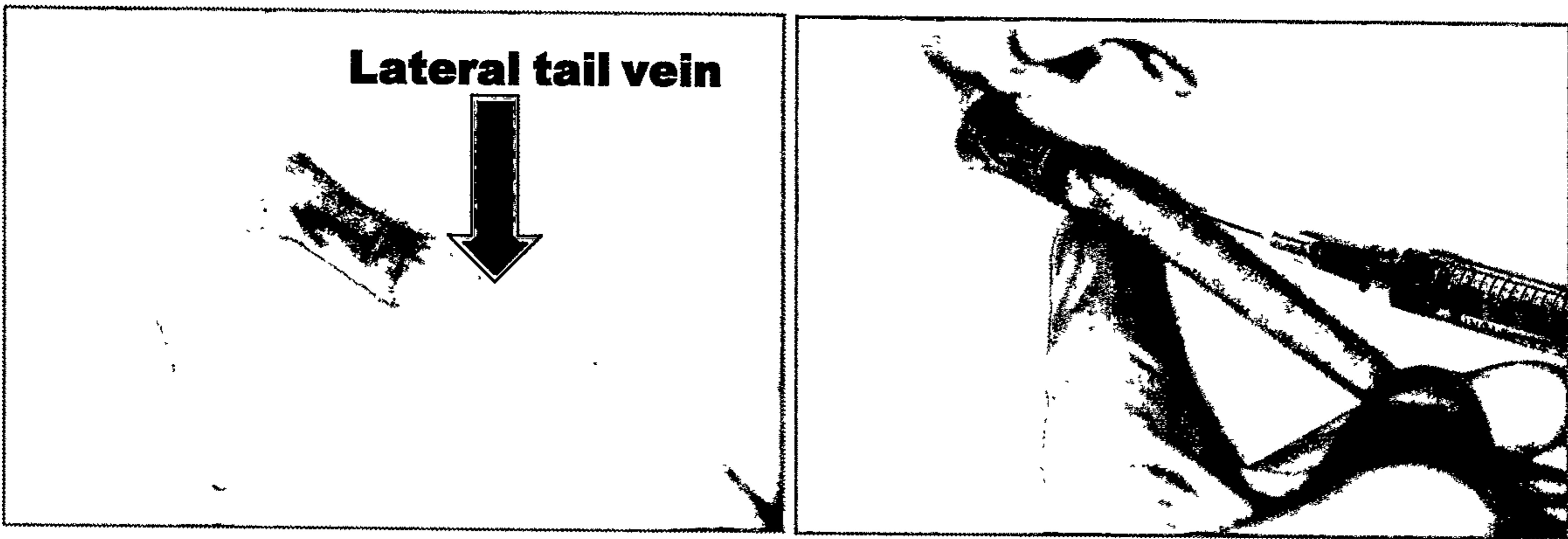


Figure 7- Repeat blood samples were taken at the same time of day due to diurnal variation in osteocalcin concentration (Lee *et al.*, 2000)

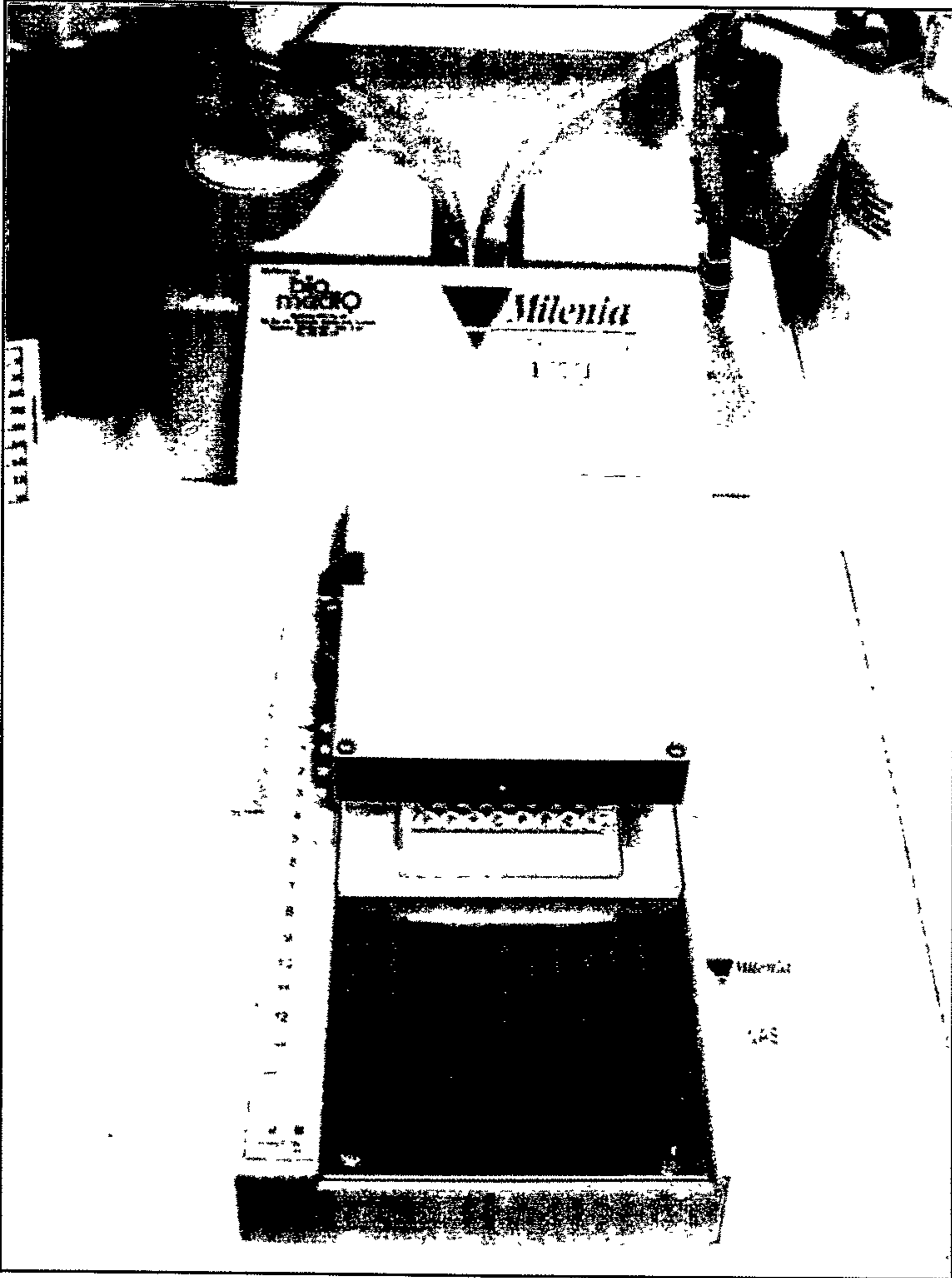


Figure 8- Plate reader preparing to read absorbance of ELISA wells at 450nm

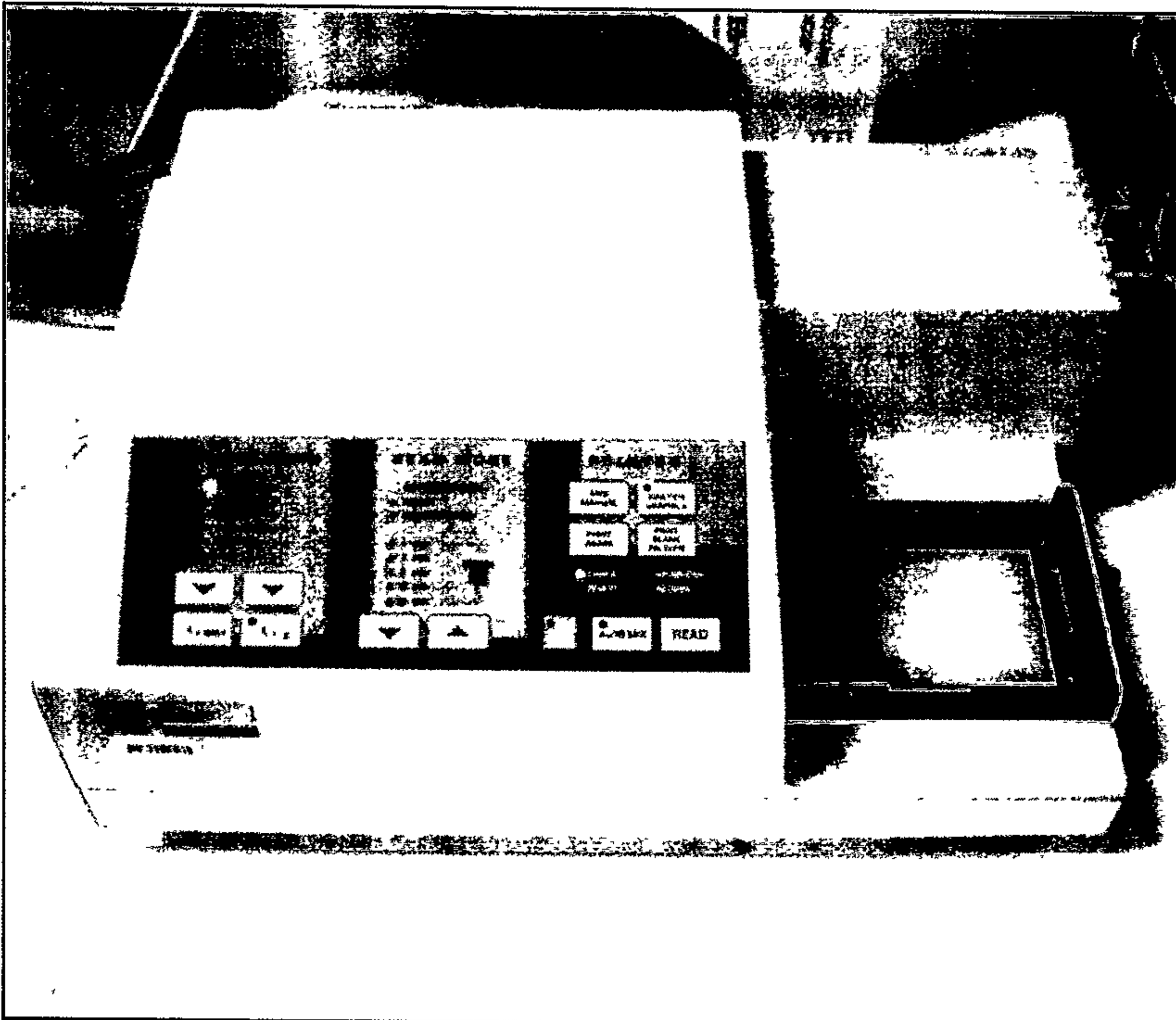
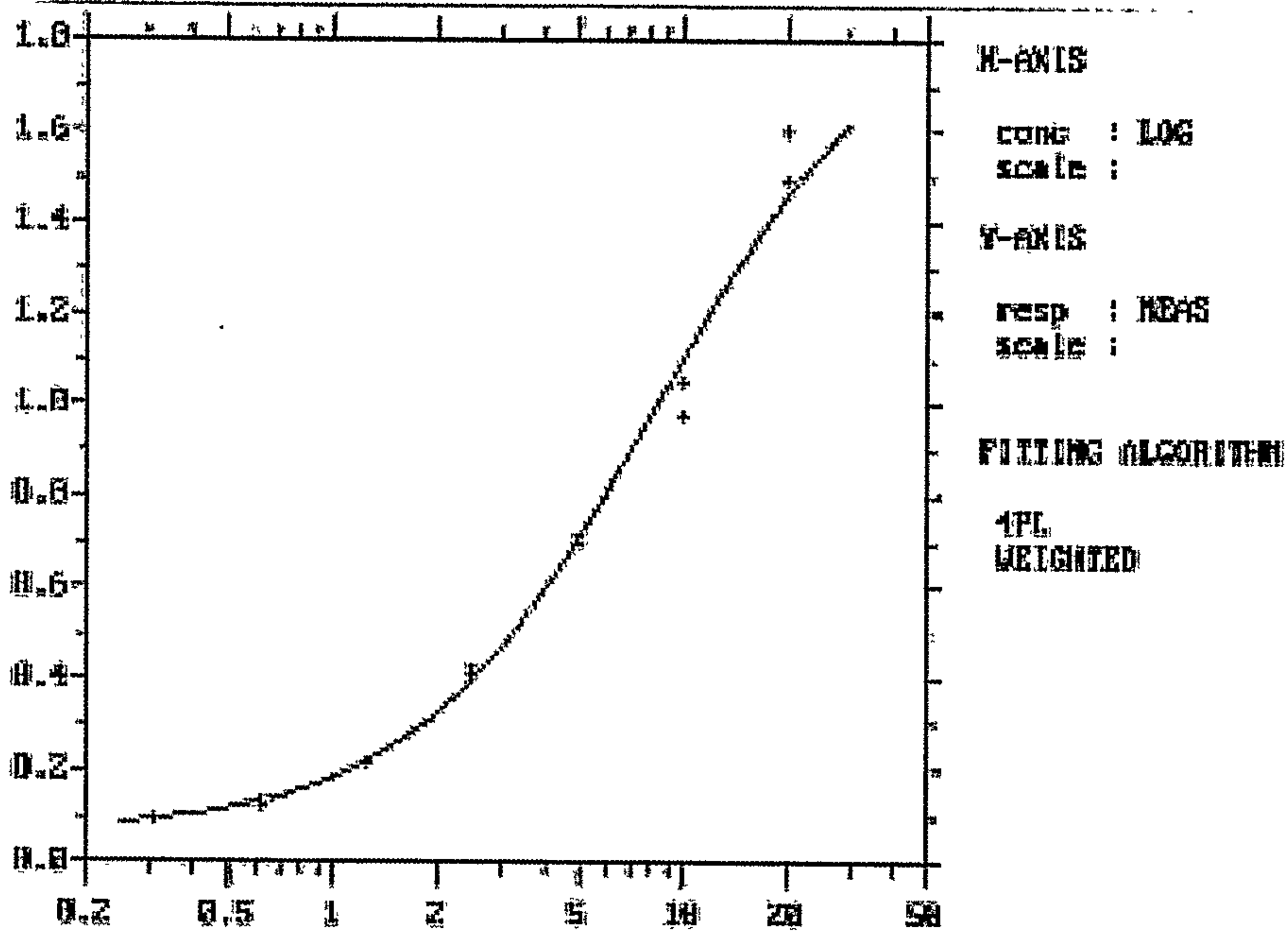


Figure 9 – Plate washing between ELISA reagents



4PL-model : resp = D + (A-D) / (1 + (conc/C)^B)

D= ESTIMATED BLANK = 0.0650
 A= ESTIMATED REFER = 1.9169
 B= SLOPE FACTOR = -1.265
 C= TURNING POINT = 8.2574

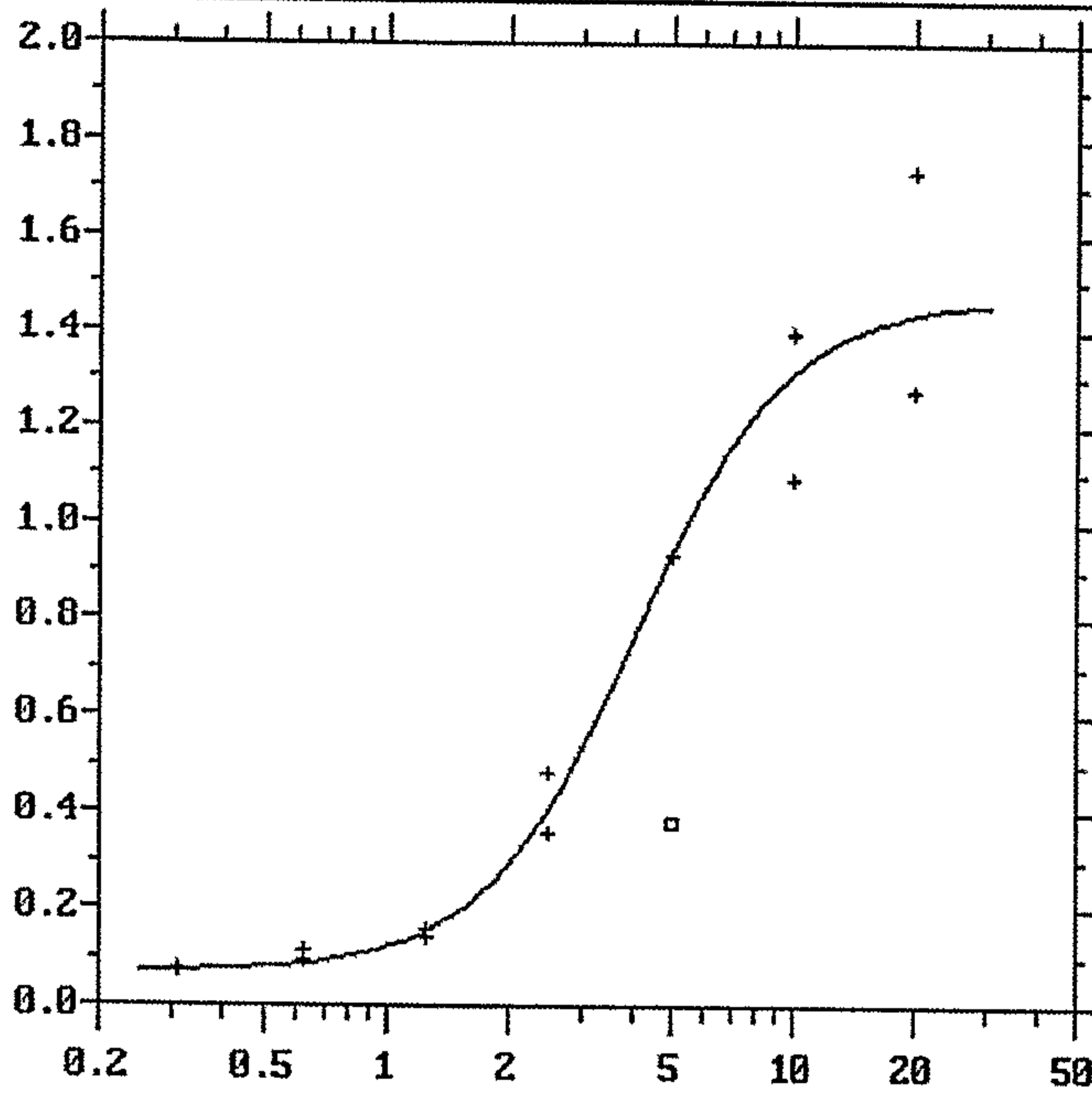
Standard Curve for
 determination of
 osteocalcin concentration
 (first ELISA kit)

BLANK = not coded (0.0650)
 REFER = not coded (1.917)

ED-20 = 2.269 ED-50 = 5.697 ED-80 = 11.61

X-AXIS (CONCENTRATION) = LOG SLOPE = 1.265
 Y-AXIS (RESPONSE) = MEAS INTERCEPT = 2.671
 FITTING ALGORITHM = 4PL /W VARIANCE RATIO = 4.083

STD	CONC	CALC.CONC	%DIFF	RESPONSE	%cvRESP	%cvCONC
1.1	0.313	0.313	0.20	0.094		
1.2	0.313	0.313	0.20	0.094		
AVG.	0.313	0.313	0.20	0.094	***** 0.02	0.01
2.1	0.625	0.669	7.08	0.139		
2.2	0.625	0.533	-14.8	0.121		
AVG.	0.625	0.602	-3.73	0.130	***** 9.79	16.1
3.1	1.250	1.252	0.19	0.221		
3.2	1.250	1.218	-2.58	0.216		
AVG.	1.250	1.235	-1.19	0.219	***** 1.62	1.99
4.1	2.500	2.669	6.78	0.423		
4.2	2.500	2.560	2.41	0.408		
AVG.	2.500	2.615	4.59	0.415	***** 2.55	2.95
5.1	5.000	5.051	1.03	0.712		
5.2	5.000	4.929	-1.42	0.699		
AVG.	5.000	4.990	-0.20	0.706	***** 1.30	1.73
6.1	10.00	8.077	-19.2	0.978		
6.2	10.00	9.151	-8.49	1.051		
AVG.	10.00	8.597	-14.0	1.015	***** 5.09	8.81
7.1	20.00	21.57	7.85	1.493		
7.2	20.00	28.74	43.7	1.600		
AVG.	20.00	24.71	23.5	1.546	***** 4.89	20.2



X-AXIS

conc : LOG
scale :

Y-AXIS

resp : MEAS
scale :

FITTING ALGORITHM

4PL
WEIGHTED

4PL-model : $resp = D + (A-D) / [1 + (conc/C)^B]$

D= ESTIMATED BLANK = 0.0687
A= ESTIMATED HEPER = 1.4681
B= SLOPE FACTOR = -2.313
C= TURNING POINT = 4.6817

BLANK = not coded (0.0687)
HEPER = not coded (1.468)

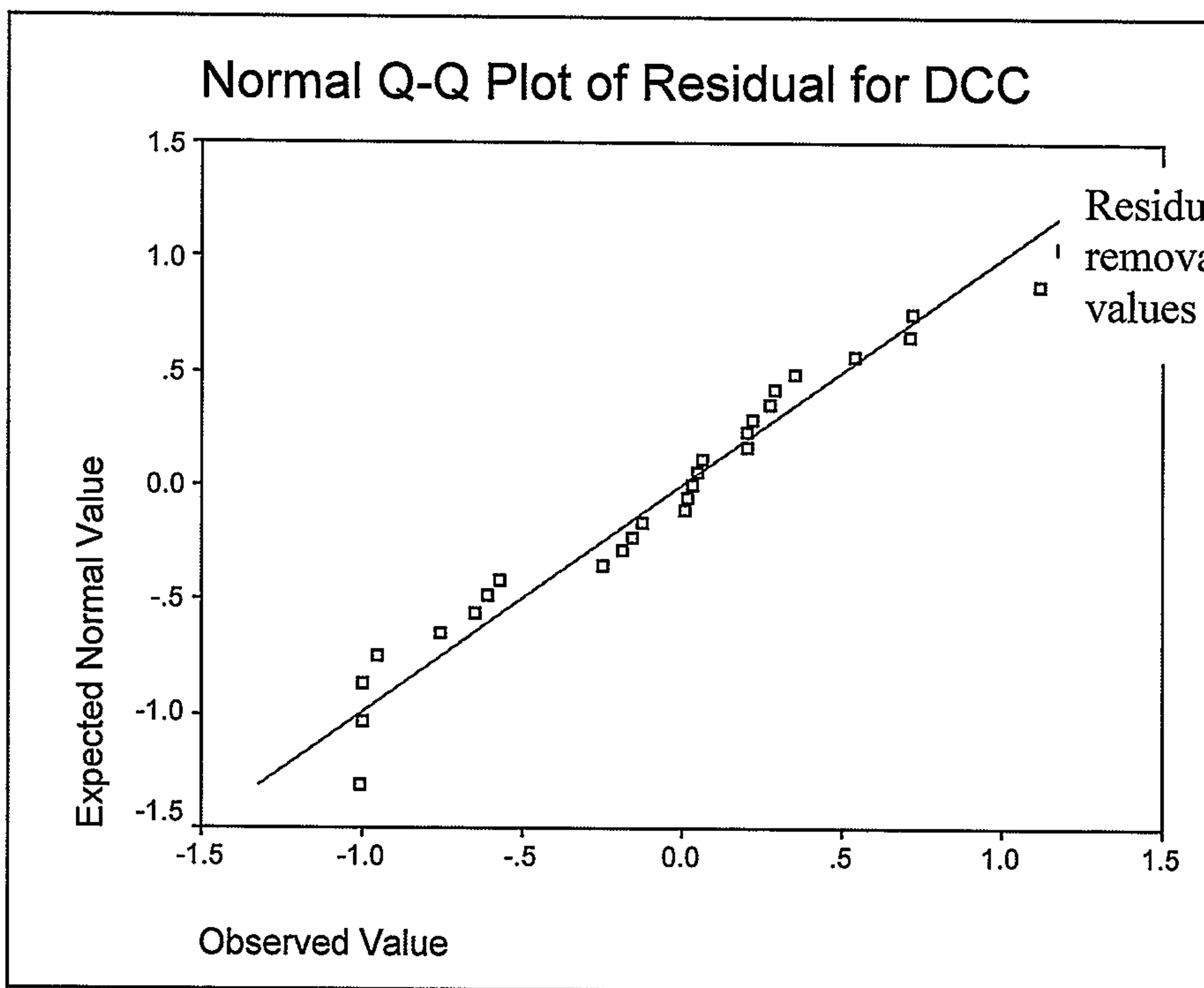
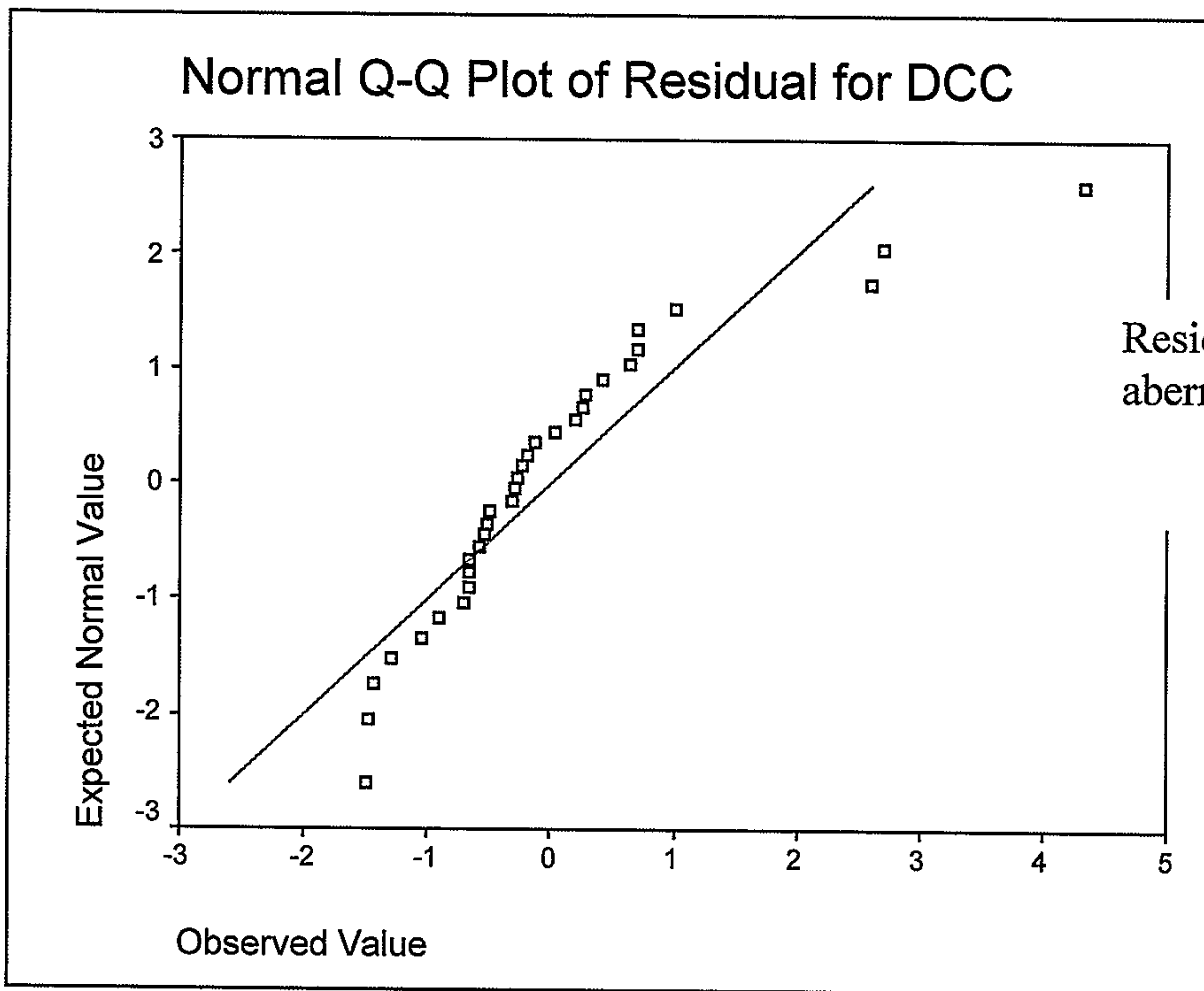
Standard Curve for
determination of
osteocalcin concentration
(second ELISA kit)

ID-20 = 2.225 ED-50 = 4.025 ED-80 = 7.068

X-AXIS (CONCENTRATION) = LOG
Y-AXIS (RESPONSE) = MEAS
FITTING ALGORITHM = 4PL /W

SLOPE = 2.313
INTERCEPT = 3.254
VARIANCE RATIO = 0.155

STD	CONC	CALC. CONC	ADIFF	RESPONSE	REVERSE	REVCONE
1.1	0.313	0.366	17.3	0.0740		
1.2	0.313	0.198	-16.5	0.0700		
AVG.	0.313	0.280	-4.41	0.0720	*****	3.93 42.1
2.1	0.625	0.700	12.0	0.092		
2.2	0.625	0.840	50.3	0.114		
2.3	0.625	0.840	50.3	0.114		
AVG.	0.625	0.830	12.8	0.103	*****	15.1 20.7
4.1	1.250	1.175	-6.02	0.143		
4.2	1.250	1.208	3.70	0.152		
AVG.	1.250	1.231	-1.52	0.151	*****	7.49 6.34
4.1	2.500	2.287	-8.53	0.159		
4.2	2.500	2.803	18.1	0.482		
AVG.	2.500	2.547	1.87	0.120	*****	20.7 14.3
5.1	5.000	5.002	0.04	0.500		
5.2	5.000	2.376	-52.5	0.300	REJECTED	
AVG.	5.000	5.002	0.04	0.500	*****	0.00 0.00
6.1	10.00	6.242	-37.6	1.087		
6.2	10.00	13.84	19.4	1.391		
AVG.	10.00	8.260	-17.4	1.232	*****	17.3 51.0
7.1	20.00	9.069837		1.736		
7.2	20.00	8.954	-55.2	1.273		
AVG.	20.00	9.009817	OUT	1.504	*****	21.8 0.00



5. Statistical Analysis

Between-Subjects Factors

	Value Label	N
FL Fluoride 0	no	16
1	yes	16
SP Springs 0	no	12
1	yes	20

Tests of Between-Subjects Effects

Dependent Variable: DCC Conc increase

Source	Type III Sum of Squares	df	Mean Square	F	Sig.
Corrected Model	14.289 ^a	3	4.763	2.728	.063
Intercept	81.089	1	81.089	46.444	.000
FL	.727	1	.727	.416	.524
SP	7.276	1	7.276	4.167	.051
FL * SP	4.903	1	4.903	2.808	.105
Error	48.887	28	1.746		
Total	163.110	32			
Corrected Total	63.175	31			

a. R Squared = .226 (Adjusted R Squared = .143)

Estimated Marginal Means

1. Fluoride

Dependent Variable: DCC Conc increase

Fluoride	Mean	Std. Error	95% Confidence Interval	
			Lower Bound	Upper Bound
0 no	1.488	.341	.790	2.187
1 yes	1.800	.341	1.101	2.499

2. Springs

Dependent Variable: DCC Conc increase

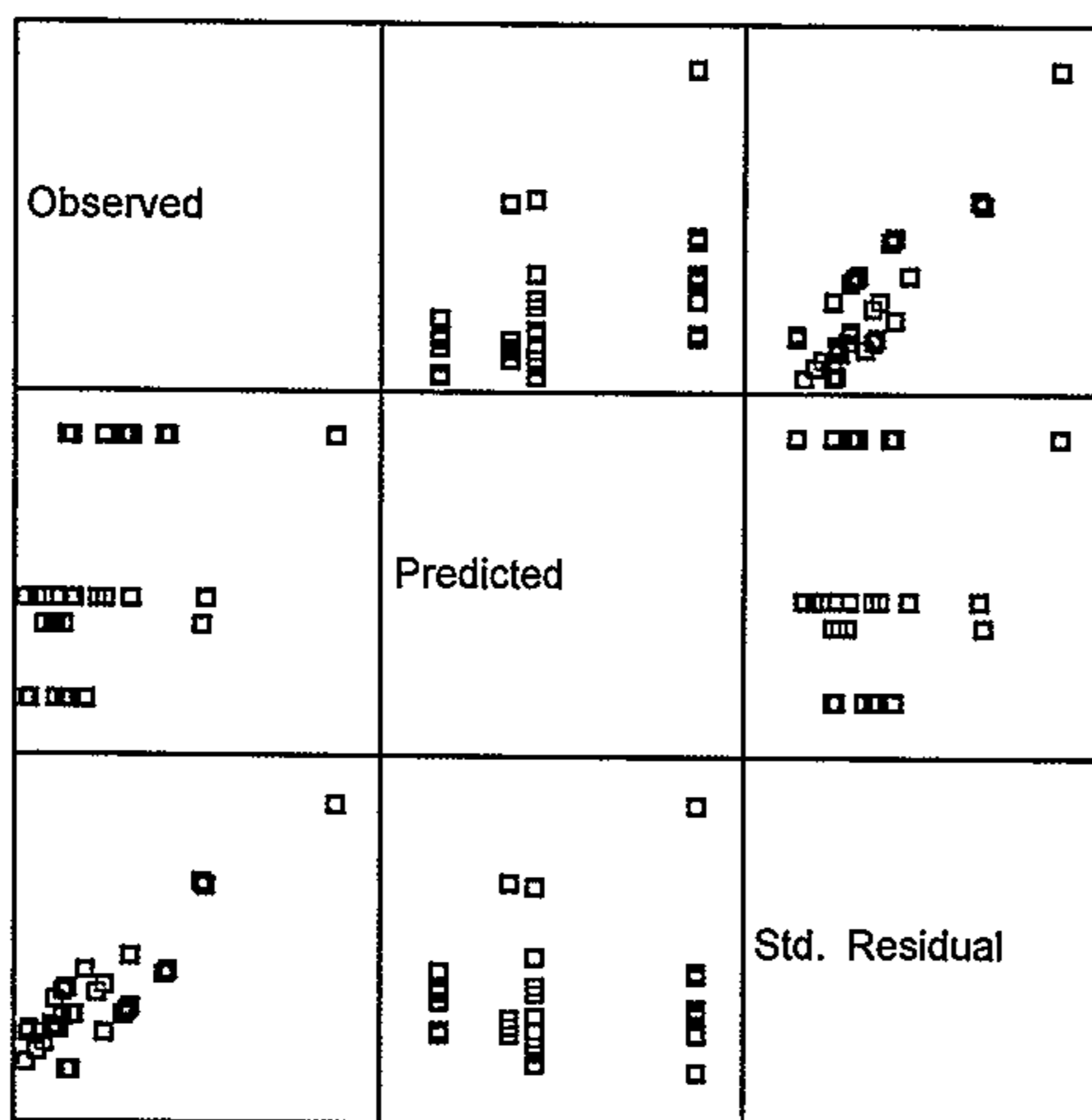
Springs	Mean	Std. Error	95% Confidence Interval	
			Lower Bound	Upper Bound
0 no	1.152	.381	.370	1.933
1 yes	2.137	.295	1.531	2.742

3. Fluoride * Springs

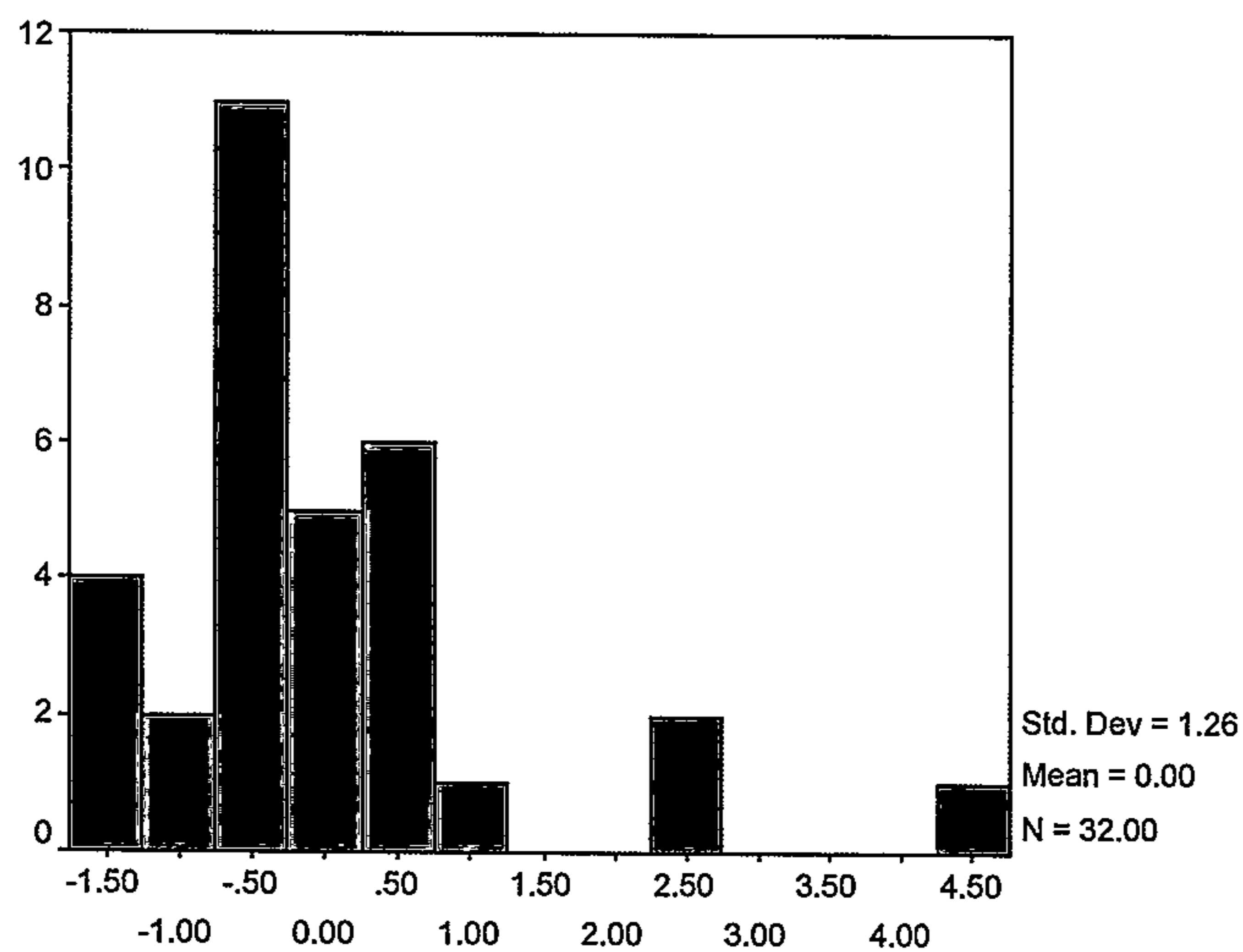
Dependent Variable: DCC Conc increase

Fluoride	Springs	Mean	Std. Error	95% Confidence Interval	
				Lower Bound	Upper Bound
0 no	0 no	1.400	.539	.295	2.505
	1 yes	1.577	.418	.721	2.433
1 yes	0 no	.903	.539	-.202	2.008
	1 yes	2.696	.418	1.841	3.552

Dependent Variable: Conc increase



Model: Intercept + FL + SP + FL*SP



Residual for DCC

Statistical Analysis with three aberrant values removed

Between-Subjects Factors

		Value Label	N
FL Fluoride	0	no	14
	1	yes	15
SP Springs	0	no	11
	1	yes	18

Tests of Between-Subjects Effects

Dependent Variable: DCC Conc increase

Source	Type III Sum of Squares	df	Mean Square	F	Sig.
Corrected Model	9.013 ^a	3	3.004	6.347	.002
Intercept	47.119	1	47.119	99.534	.000
FL	1.595	1	1.595	3.369	.078
SP	5.132	1	5.132	10.840	.003
FL * SP	1.334	1	1.334	2.818	.106
Error	11.835	25	.473		
Total	79.531	29			
Corrected Total	20.848	28			

a. R Squared = .432 (Adjusted R Squared = .364)

Estimated Marginal Means

1. Fluoride

Dependent Variable: DCC Conc increase

Fluoride	Mean	Std. Error	95% Confidence Interval	
			Lower Bound	Upper Bound
0 no	1.075	.192	.679	1.470
1 yes	1.559	.181	1.186	1.933

2. Springs

Dependent Variable: DCC Conc increase

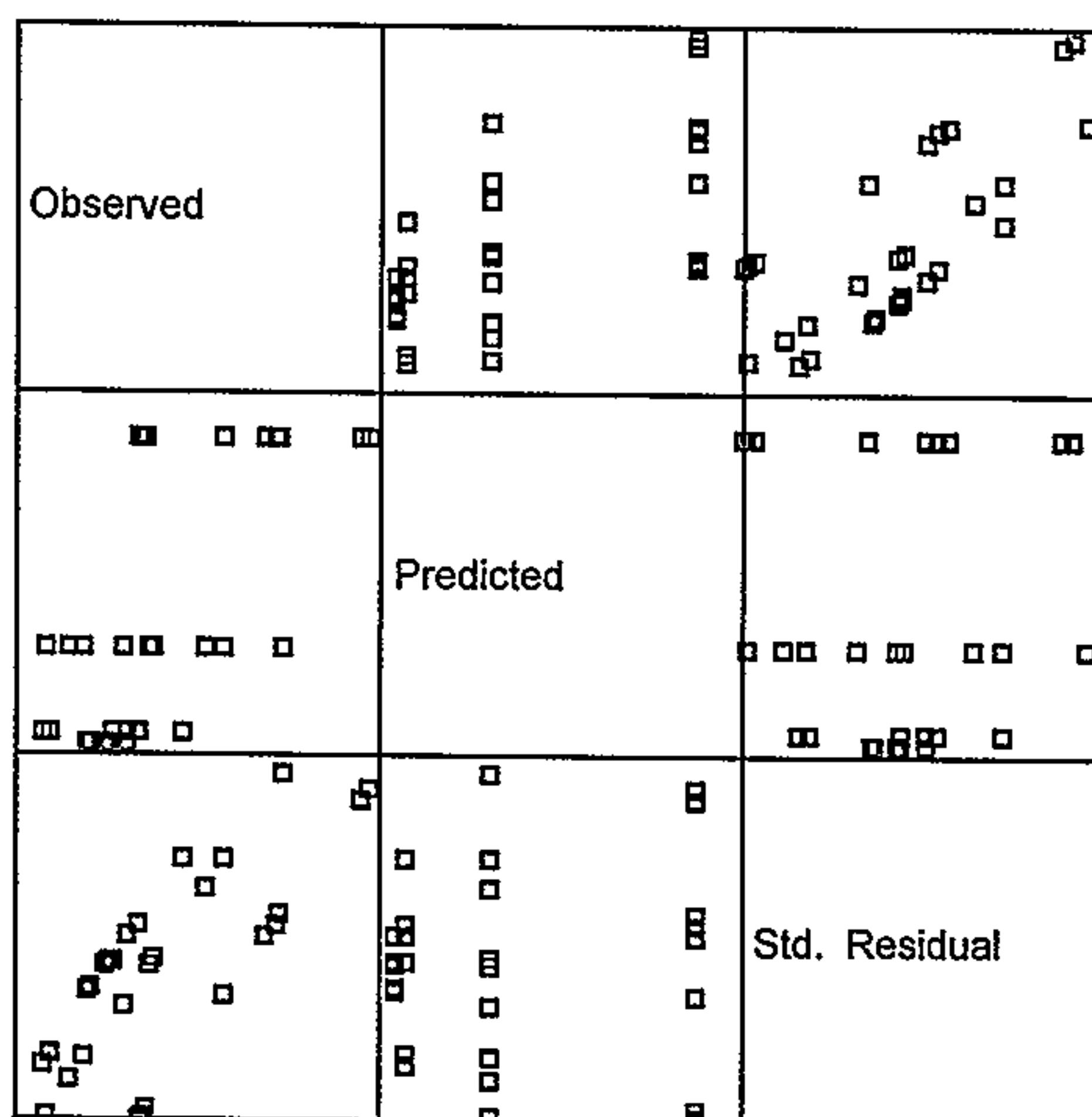
Springs	Mean	Std. Error	95% Confidence Interval	
			Lower Bound	Upper Bound
0 no	.882	.208	.453	1.311
1 yes	1.751	.162	1.418	2.085

3. Fluoride * Springs

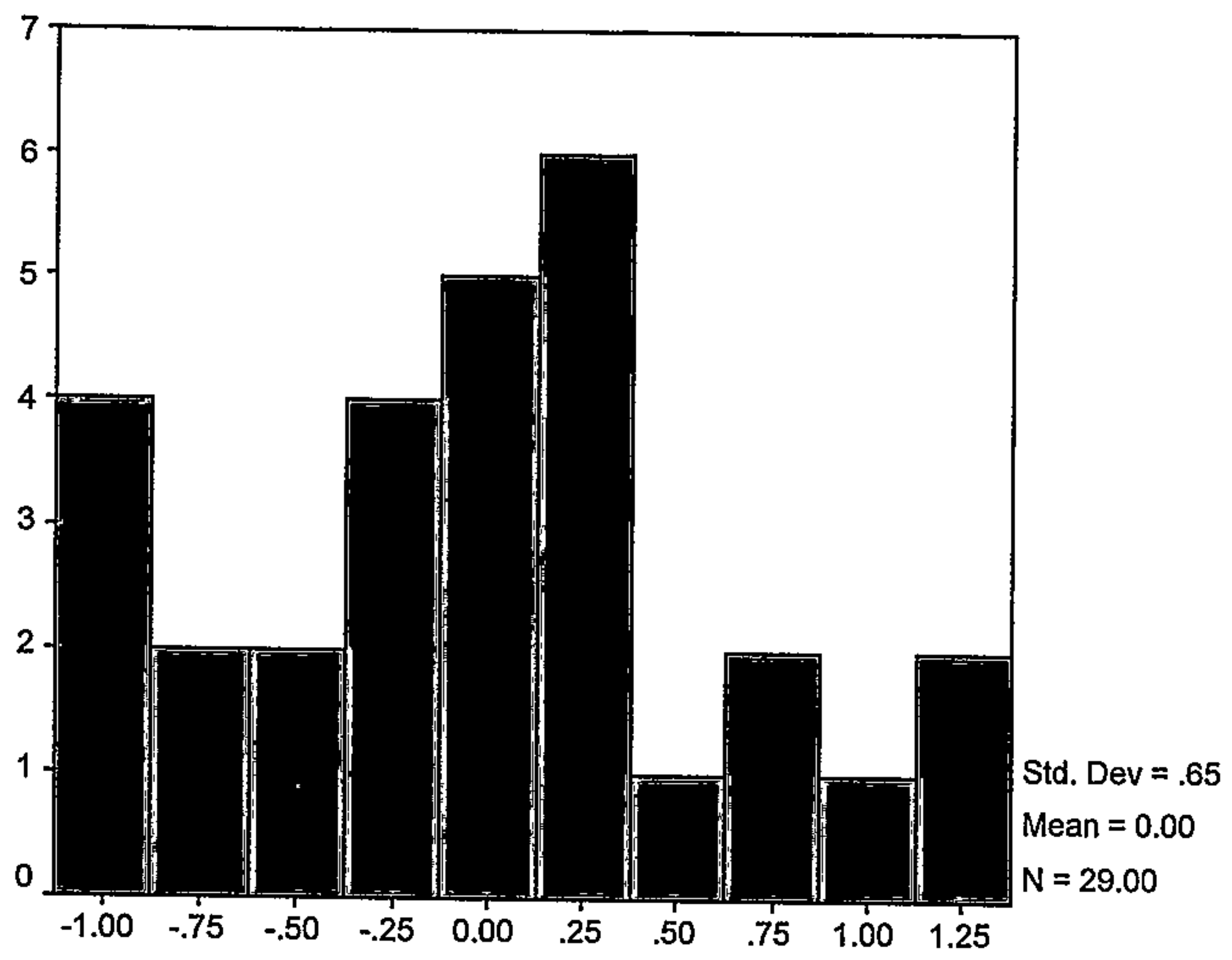
Dependent Variable: DCC Conc increase

Fluoride	Springs	Mean	Std. Error	95% Confidence Interval	
				Lower Bound	Upper Bound
0 no	0 no	.862	.308	.228	1.495
	1 yes	1.288	.229	.815	1.760
1 yes	0 no	.903	.281	.324	1.482
	1 yes	2.215	.229	1.743	2.688

Dependent Variable: Conc increase



Model: Intercept + FL + SP + FL*SP



Residual for DCC

6. Appendix – ELISA Data

Sequence	Absorb	Conc	%CV	Unit ng/ml	Seq	Absorb	Conc	%CV
A1	0.591	3.976			A10	1.093	6.301	
	0.634	4.343				0.559	3.126	
mean	0.613	4.159	6.2			0.826	4.713	47.6
	1	0.813	6.071		10	1.106	6.433	
		0.797	5.901			1.156	7.001	
		0.805	5.986	2		1.131	6.717	6
A2	0.648	4.466			A9	0.536	3.028	
	0.543	3.584				0.753	4.005	
	0.595	4.025	15.5			0.645	3.517	19.6
	2	0.633	4.334		9	0.937	5.048	
		0.682	4.772			1.168	7.154	
		0.658	4.553	6.8		1.053	6.101	24.4
A3	0.478	3.079			J	0.8	4.244	
	0.494	3.201				0.944	5.095	
	0.486	3.14	2.7			0.872	4.669	12.9
	3	0.615	4.179		J	1.057	5.963	
		0.673	4.689			1.05	5.902	
		0.644	4.434	8.1		1.053	5.933	0.7
A5	0.664	4.608			I	0.745	3.965	
	0.653	4.51				0.964	5.232	
	0.658	4.559	1.5			0.854	4.599	19.5
	5	0.882	6.85		I	1.046	5.867	
		0.634	4.343			1.316	10.135	
		0.758	5.596	31.7		1.181	8.001	37.7
A7	0.625	4.265			C4	0.869	4.626	
	0.655	4.528				0.849	4.511	
	0.64	4.396	4.2			0.859	4.568	1.8
	7	0.981	8.119		C4	0.867	4.614	
		1.043	9.026			1.054	5.937	
		1.012	8.573	7.5		0.961	5.276	17.7
A8	0.538	3.544			C5	1.018	5.635	

	0.728	5.204			1.098	6.351	
	0.633	4.374	26.8		1.058	5.993	8.4
8	1.043	9.026		<u>C5</u>	0.936	5.041	
	0.389	2.423			1.261	8.698	
	0.716	5.725	81.6		1.099	6.87	37.6
A	0.335	2.041		C6	0.804	4.265	
	0.355	2.182			0.722	3.854	
	0.345	2.112	4.7		0.763	4.06	7.2
A	0.597	4.026		<u>C6</u>	0.83	4.405	
	0.728	5.204			1.005	5.553	
	0.663	4.615	18		0.918	4.969	16.1
B	0.344	2.104		CD	0.601	3.305	
	0.282	1.673			0.724	3.863	
	0.313	1.889	16.1		0.663	3.584	11
B	0.616	4.187		<u>CD</u>	0.667	3.598	
	0.676	4.717			0.798	4.234	
	0.646	4.452	8.4		0.732	3.916	11.5
C	0.48	3.094		CE	1.08	6.175	
	0.558	3.705			1.04	5.816	
	0.519	3.399	12.7		1.06	5.995	4.2
C	0.755	5.47		<u>CE</u>	1.264	8.763	
	0.822	6.168			1.012	5.588	
	0.789	5.819	8.5		1.138	7.175	31.3
D	0.308	1.853		CF	0.692	3.713	
	0.416	2.618			0.846	4.494	
	0.362	2.236	24.2		0.769	4.103	13.5
D	1.032	8.858		<u>CF</u>	0.995	5.457	
	1.083	9.669			1.059	5.981	
	1.057	9.263	6.2		1.027	5.719	6.5
E	0.392	2.445					
	0.434	2.75					
	0.413	2.598	8.3				
E	0.539	3.552					
	0.603	4.077					
	0.571	3.815	9.7				
F	0.423	2.669					

	0.35 2.147	
	0.387 2.408	15.4
E	0.783 5.754	
	0.781 5.734	
	0.782 5.744	0.3
G	0.491 3.178	
	0.531 3.489	
	0.511 3.333	6.6
<u>G</u>	0.663 4.599	
	0.649 4.474	
	0.656 4.537	1.9
H	0.576 3.852	
	0.562 3.737	
	0.569 3.795	2.1
<u>H</u>	0.716 5.089	
	0.857 6.559	
	0.786 5.824	17.8
C1	0.319 1.93	
	0.459 2.936	
	0.389 2.433	29.2
<u>C1</u>	0.9 7.067	
	0.805 5.985	
	0.852 6.526	11.7
C2	0.304 1.826	
	0.318 1.923	
	0.311 1.874	3.7
<u>C2</u>	0.524 3.434	
	0.396 2.474	
	0.46 2.954	23
C3	0.417 2.626	
	0.391 2.438	
	0.404 2.532	5.2
<u>C3</u>	0.509 3.317	
	0.496 3.216	
	0.502 3.266	2.2
CA	0.316 1.909	

		0.296	1.77	
		0.306	1.84	5.3
<u>CA</u>		0.468	3.003	
		0.452	2.883	
		0.46	2.943	2.9
<u>CB</u>		0.313	1.888	
		0.349	2.14	
		0.331	2.014	8.8
<u>CB</u>		0.465	2.981	
		0.456	2.913	
		0.461	2.947	1.6
<u>CC</u>		0.631	4.317	
		0.598	4.035	
		0.614	4.176	4.8
<u>CC</u>		0.589	3.96	
		0.696	4.901	
		0.642	4.43	15
Sample 2				
A4		0.601	3.987	
		0.578	3.785	
		0.589	3.886	3.6
	4	0.627	4.238	
		0.614	4.108	
		0.62	4.173	2.2
A6		0.609	4.068	
		0.636	4.328	
		0.623	4.198	4.4
	6	0.684	4.833	
		0.691	4.917	
		0.688	4.875	1.2

LEGEND

Fluoridated sample	A
Post-mortem	<u>A</u>
Non-fluoridated sample	1
Post-mortem	<u>1</u>
Control (fluoride)	CA
Post-mortem	<u>CA</u>
Control (non-fluoride)	C1
Post-mortem	<u>C1</u>
Conc	- Concentration of osteocalcin
CV	- Coefficient of variation
Absorb	- Absorbance at 450 nm

The pain passes. The beauty remains.

Pierre-Auguste Renoir